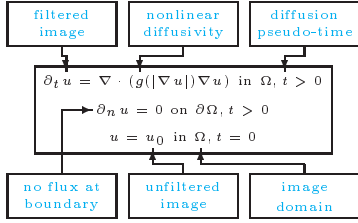


Nonlinear Anisotropic Diffusion Filters for Wide Range Edge Sharpening

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Nonlinear Anisotropic Diffusion



Scalar $g(|\nabla u|) \geq 0$ increases/decreases diffusion for small/large $|\nabla u|$.

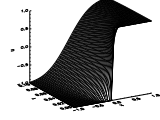
Objectives

- improve images **qualitatively**,
- remove **noise**,
- preserve **details** and even: **enhance edges**.

Blurring and Sharpening Models

Blurring by **forward** diffusion:
 $\partial_t u = +\nabla^2 u$.

Example: $u(x, t) = \text{Erf}\left(\frac{x}{2\sqrt{t}}\right)$



Sharpening by **backward** diffusion:

$$\partial_t u = -\nabla^2 u.$$

Backward diffusion is **unstable**!

Nonlinear Models can be Stable

The 1D problem:

$$\begin{aligned} u_t &= -|u_x|u_{xx} \text{ in } \Omega, t > 0 \\ u_n &= 0 \text{ on } \partial\Omega, t > 0 \\ u &= u_0 \text{ in } \Omega, t = 0 \end{aligned}$$

is **well-posed**! [Osher & Rudin, 90]

Defining the **flux**:

$$\Phi(s) = sg(s)$$

the general PDE can be written:

$$u_t = \frac{\Phi'(|\nabla u|)u_{nn}}{|\nabla u|} + g(|\nabla u|)[\nabla^2 u - u_{nn}]$$

Diffusion normal to level sets of u .
Backward if $\Phi' < 0$.

Diffusion tangent to level sets of u .
Forward: $g \geq 0$.

Diffusion is **anisotropic**:



Forward underlying backward diffusion.

Approaches to Edge Enhancement

Shock Filtering [Osher & Rudin, 90]:

$$\partial_t u = -|\nabla u|F(\mathcal{L}(u))$$

$$\text{sign}(F(s)) = \text{sign}(s), \mathcal{L}(u) \sim u_{nn}$$

Based upon level set methods.

Variational Filtering:

$$\min_u J(u) = \int_{\Omega} \phi(|\nabla u|) + \frac{\kappa}{2} \int_{\Omega} |u_0 - u|^2$$

Optimality condition in steady state:

$$\partial_t u = \nabla \cdot \left(\frac{\phi'(|\nabla u|)}{|\nabla u|} \nabla u \right) + \nu(u_0 - u)$$

- Gaussian [Tikhonov & Arsenin, 77]:

$$\phi(s) = \frac{1}{2}s^2$$

- Total Variation (TV) [Rudin et al., 92]:

$$\phi(s) = s$$

- Unification [Nordström, 90]:

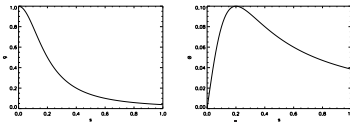
$$\phi'(s) = \Phi(s) = sg(s)$$

ϕ **convex/concave** where $\phi'' = \Phi' > / < 0$.

Perona-Malik Filters

$$\partial_t u = \nabla \cdot (g(|\nabla u|) \nabla u)$$

- Diffusivity $g(s)$ is **bell-shaped**.
- Flux $\Phi(s) = sg(s)$ **increases** then **decreases**.



Normal diffusion **forward** for $|\nabla u| < \lambda$.

Normal diffusion **backward** for $|\nabla u| > \lambda$.

Tangential diffusion **forward** for $|\nabla u| \geq 0$.

- Perona-Malik Paradox:

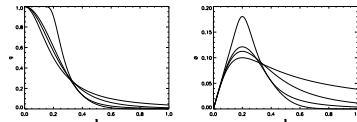
Technical ill-posedness—see references.

Numerics stable—besides staircasing.

- Regularizations**: [Catté et al., 92] spatial,

$$\partial_t u = \nabla \cdot (g(|\nabla u_{\sigma}|) \nabla u), u_{\sigma} = K_{\sigma} * u.$$

Established Perona-Malik Filters



$$\text{PM1: } \left[1 + \left(\frac{s}{\lambda}\right)^2\right]^{-1} \text{ [Perona \& Malik, 87]}$$

$$\text{GR: } \left[1 + \frac{1}{3} \left(\frac{s}{\lambda}\right)^2\right]^{-2} \text{ [Geman \& Reynolds, 92]}$$

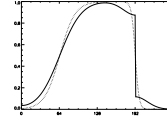
$$\text{PM2: } \exp\left[-\frac{1}{2} \left(\frac{s}{\lambda}\right)^2\right] \text{ [Perona \& Malik, 87]}$$

$$\text{W: } 1 - \exp\left[-\gamma \left(\frac{s}{\lambda}\right)^4\right] \text{ [Weickert, 98]}$$

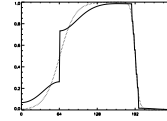
More **rapid/gradual** decay: **longer/briefer** sharpening over **narrower/wider** range.

Sensitivity to Parameters

PM2: Very **precise** tuning of λ required to sharpen a given edge.



Weaker edge **smoothed**.



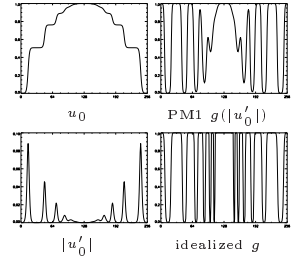
Stronger edge **staircased**.

Continuum analysis predicts sharpening

only for $\lambda \leq |u_x| \leq \chi = \lambda\sqrt{3}$

where $\Phi'(\lambda) = 0$ and $\Phi''(\chi) = 0$.

Test Problem



u_0 is sum of six: $a(1 + bx^2)^{-c}$.
Cannot use PM to sharpen all edges.

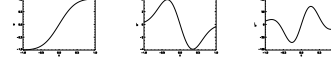
Two methods to fix:

- adjust λ locally,
- scale $|u_x|$ locally.

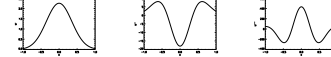
Success in 1D, not robust in 2D.

Limits of Edge Enhancement

Even edge derivatives vanish:



Odd edge derivatives alternate in sign:



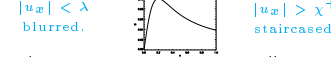
Sharpening requires: $(\Phi' < 0, \Phi'' < 0?)$

$$\partial_t u = 0$$

$$\partial_t u_x = \Phi' u_{xx} > 0$$

$$\partial_t u_{xx} = 0$$

$$\partial_t u_{xxx} = 3\Phi'' u_{xxx}^2 + \Phi' u_{xxxx} < 0$$



$$\Phi'(\lambda) = 0 \quad \lambda \chi \quad \Phi''(\chi) = 0$$

$\lambda < |u_x| < \chi$ sharpened.

In practice: **same** (λ, χ) , **different** results.

Widely Sharpening Filters

- Speculation from computations:

need **uniformly**: $\Phi'(s) \sim -1$.

- Success in 1D, excess smoothing in 2D:

unbalanced: $\Phi'(s) = -1, g(s) = \mathcal{O}(\frac{1}{s})$.

- Experiments with $g(s) = s^{-p}$:

$p > 2$ unstable, **$p = 2$ excellent!**

- No accident:

$$-1 = \frac{\Phi'(s)}{g(s)} \Rightarrow g(s) = \frac{1}{s^2}$$

Balanced Forward-Backward (BFB).

- Treatment of noise:

$$-\frac{s}{\kappa+s} = \frac{\Phi'(s)}{g(s)} \Rightarrow g(s) = \frac{1}{s(\kappa+s)}$$

Gradually Balanced Forward-Backward (GBFB).

$$\text{GBFB} \left[\frac{1}{s(\kappa+s)} \right] : \text{TV} \left[\frac{1}{s} \right] \rightarrow \text{BFB} \left[\frac{1}{s^2} \right].$$

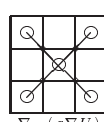
- BFB & GBFB are **unbalanced**:

$$\phi''(s) = \Phi'(s) < 0.$$

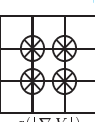
Numerical Discretization

- Spatial discretization:

$$h^2 \nabla \cdot (g(|\nabla V|) \nabla U)_{i,j} = [G(V)U]_{i,j}$$



$$\nabla \cdot (g \nabla U)$$



$$g(|\nabla V|)$$

Diagonal less dissipative

- Temporal discretization: $\mu = \tau h^{-2}$

Explicit: (PM, $\mu \leq \frac{1}{2}$)

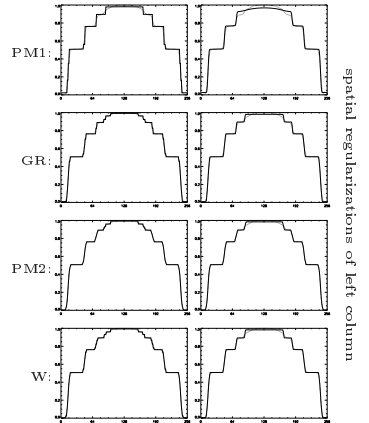
$$U^{n+1} = [I + \mu G(U^n)] U^n$$

Semi-implicit: (BFB & GBFB)

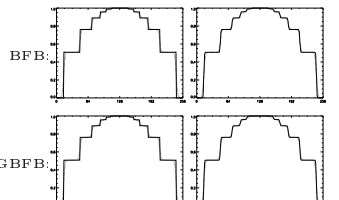
$$[I - \mu G(U^n)] U^{n+1} = U^n$$

Solved inexpensively by Jacobi preconditioned conjugate gradient.

Perona-Malik Filters in 1D



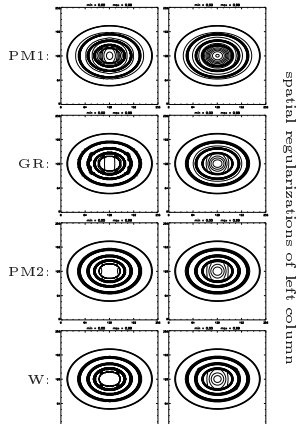
Concave Filters in 1D



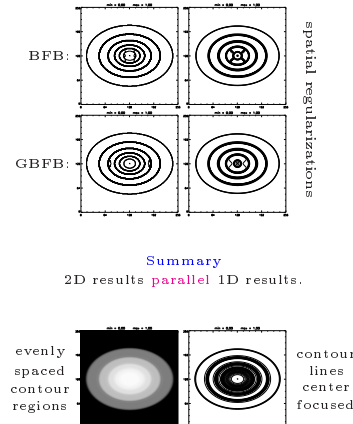
Summary

- Perona-Malik filters:
 - only one** edge pair accurate,
 - PM1** best (parameter limit: **BFB**).
- Concave filters:
 - all edges** sharpened well,
 - rapid** and **simultaneous** sharpening.
- Spatial regularization (for both):
 - rounds** steps (and 2D level curves),
 - flattens** small-slope regions,
 - retards** edge sharpening.

Perona-Malik Filters in 2D

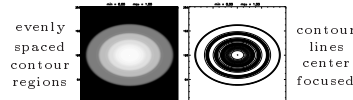


Concave Filters in 2D



Summary

2D results **parallel** 1D results.



Noisy HR MRI of *in vitro* AS vessel

