

Cardiovascular Simulations

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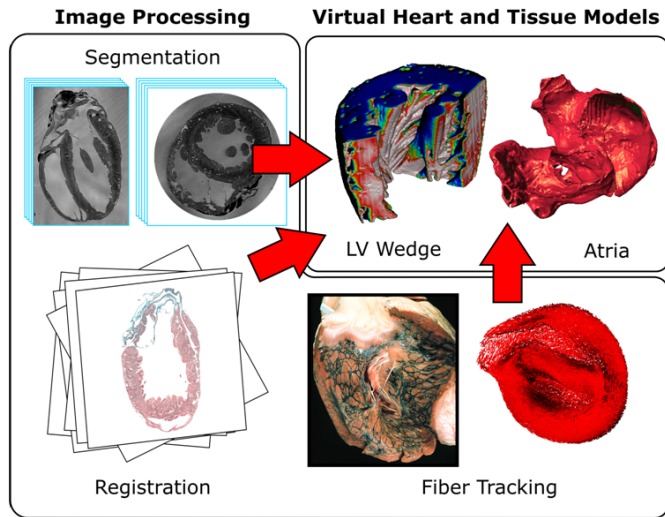
MONT-BLANC



BioTechMed[®]
GRAZ

Video

Virtual heart [SFB: G. Plank]



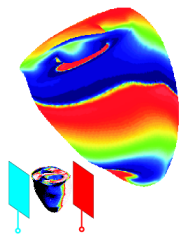
Virtual heart - goals in CARP project [G.Plank]

Gernot Plank [Graz → John Hopkins (Baltimore) → Oxford → Graz]
Ed Vigmond [Calgary → Bordeaux]

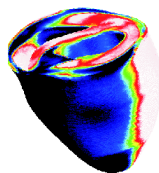
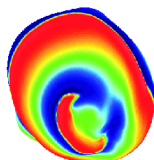
- **Simulation** of electrical stimulation of virtual heart.
- **Including** mechanics of the heart.
- **Shape** the electrical pulse wrt. certain criteria.
- Goal: **Minimize** the overall energy of the pulse for curing arrhythmia.
- Benefits:
 - ▶ **Less** internal **burnings** when internal pace makers send electrical pulses against arrhythmia.
 - ▶ **Surgery planning** for scared over tissue after a heart attack.

Rabbit Heart [G. Plank: CARP]

Reentry Induction in a Rabbit Ventricular Model



VEP Patterns



- time-dependent electrical potential, anisotropic coefficients + Purkinje fibers in bidomain equations: non-linear system of PDEs and ODEs
- 5.082.272 tetrahedrons with 862.525 FEM-nodes
- Goal: 150 Mill. tetrahedrons using parallel mesh generator Spider by F. Kickingner results in 25 Mill. d.o.f.

Rabbit Heart: bidomain equations

Two components of the electric propagation in the heart:

- ionic flux through the cell membrane: ODEs (3) accounts for over 20 variables,
- electrical model for the tissues: linear PDEs (1)–(2)

$$\nabla \cdot (\bar{\sigma}_i + \bar{\sigma}_e) \nabla V_e = -\nabla \cdot \bar{\sigma}_i \nabla V_m \quad (1)$$

$$\nabla \cdot \bar{\sigma}_i \nabla V_m = -\nabla \cdot \bar{\sigma}_i \nabla V_e + \beta I_m \quad (2)$$

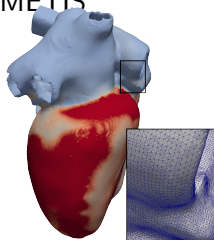
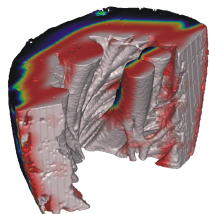
$$I_m = C_m \frac{\partial V_m}{\partial t} + I_{ion}(V_m, v) \quad (3)$$

- $\bar{\sigma}_i, \bar{\sigma}_e$: intracellular and extracellular conductivity tensors,
- β : surface to volume ratio of the cardiac cells,
- C_m : membrane capacitance per unit area,
- V_m transmembrane voltage,
- I_{ion} : ionic current density flowing through the membrane ionic channel and depends on the transmembrane voltage

Coupled system (1)–(3) is non-linear

Rabbit Heart: Discretization

- Mesh generation by spider/tarantula [F. Kickingger]
- Finite element mesh with tetrahedral and hexahedral elements
- Mesh decomposition by METIS



- Solve linear system of equations (**That is our part!**)

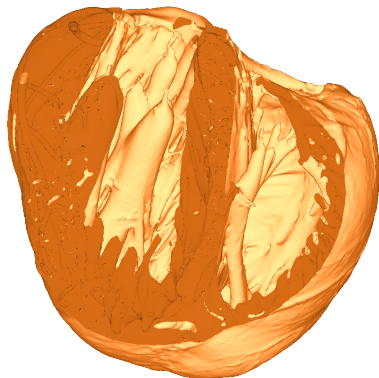
$$Ku = f$$

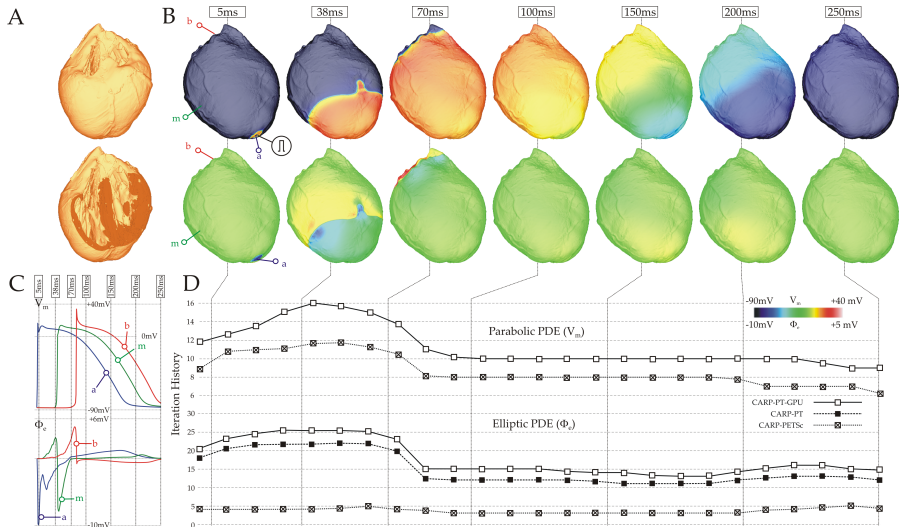
in each outer (time/non-linear) iteration.

- System matrix K is **sparse** but **unstructured**.

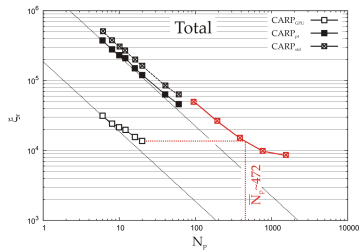
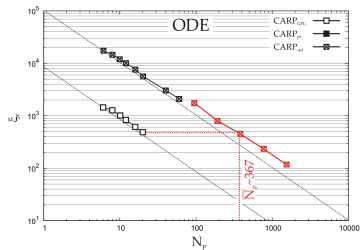
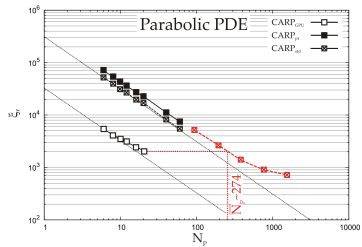
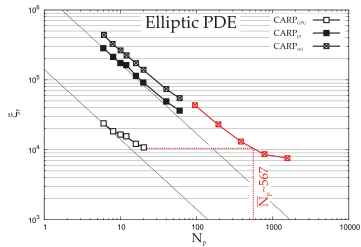
Oxford Benchmark

40.992.163 Elements; 6.901.583 d.o.f; real time duration: 250 ms





toolbox (CPU \blacksquare /GPU \square) vs. Petsc (hypr) \boxtimes on mephisto and hector [II/2012]



Strong scaling results on mephisto in sec. [II/2012]

6.9 Mill. DoFs; potential problem

Mephisto cluster: 5×2 Xeon X5650 CPUs, 60 cores at 2.67GHz;
 5×4 NVidia Tesla 2070

N	CARP-PETSc	CARP-PT-GPU	Eff. PETSc	Eff. PT	Speedup
6	126,897	8,266	1	1	15.3
8	95,057	6,519	1	0.95	14.6
10	76,060	5,667	1	0.87	13.4
12	66,134	5,586	0.96	0.73	11.8
16	49,842	4,479	0.95	0.69	11.1
20	40,523	3,807	0.93	0.65	10.6

A first summary

- GPU/CPU-MG scales very well for small/medium size parallel computers
- Usage of GPU pays off, even for **unstructured data**
- Redesign of communication also for hierarchical communication
- extension to elasticity solver?
- non-linear problems?
- Use of `#pragma`-driven parallelization for general manycore environments?.