

# Total variation regularized nonlinear inversion for parallel MRI with variable density sampling patterns

Christian Clason<sup>1</sup>    Florian Knoll<sup>2</sup>

<sup>1</sup>Institute for Mathematics and Scientific Computing, Karl-Franzens-Universität Graz

<sup>2</sup>Institute of Medical Engineering, Graz University of Technology

Workshop on Novel Reconstruction Strategies in NMR and MRI  
Göttingen, September 11, 2010

- 1 Nonlinear inversion
- 2 Variable density sampling patterns
- 3 IRGN with TV regularization
- 4 Example reconstructions
- 5 IRGN with TGV regularization

# Parallel MRI as inverse problem

**Given**

- sampling operator  $\mathcal{F}_s$  (defined by trajectory)
- acquired  $k$ -space coil data  $g = (g_1, \dots, g_N)^T$

**Find**

- spin density  $u$
- coil sensitivities  $c = (c_1, \dots, c_N)^T$

such that

$$F(u, c) := (\mathcal{F}_s(u \cdot c_1), \dots, \mathcal{F}_s(u \cdot c_N))^T = g$$

**nonlinear** inverse problem, ill-posed  $\rightsquigarrow$  solve using IRGN method

# Iteratively regularized Gauß-Newton method

- 1: Choose  $x^0 = (u^0, c^0)$ ,  $\alpha_0$ ,  $q < 1$
- 2: **repeat**
- 3:     Solve for  $\delta x = (\delta u, \delta c)$  (e.g., by CG on normal equations)

$$\begin{aligned} \min_{\delta x} \frac{1}{2} \|F'(x^k)\delta x + F(x^k) - g\|^2 + \frac{\alpha_k}{2} \|W(c^k + \delta c)\|^2 \\ + \frac{\alpha_k}{2} \|u^k + \delta u\|^2 \end{aligned}$$

- 4:     Set  $x^{k+1} = x^k + \delta x$ ,  $\alpha_{k+1} = \alpha_k q$ ,  $k = k + 1$
- 5: **until**  $\|F(x^k) - g\| < tol$

$W$  high-order differential operator (enforces smooth sensitivities)  
 $F'$  Fréchet derivative with adjoint  $F'^*$

# Nonlinear inverse problem approach

Advantage:

Flexibility in

- Sampling strategy (choice of  $\mathcal{F}_S$ )
- Incorporation of a priori information (choice of penalty)
- Minimization method (choice of gradient descent method requiring only application of  $\mathcal{F}_s, \mathcal{F}_s^T$ )

Disadvantage:

Can be less efficient than specialized methods

# Choice of sampling strategy

Trajectory should:

- 1 Minimize acquisition time  
~~> traverse only part of  $k$ -space
- 2 Minimize subsampling artifacts  
~~> denser sampling of center of  $k$ -space (auto-calibration)
- 3 Allow fast reconstruction  
~~> availability of (N)FFT

Here:

- radial sampling
- adapted Cartesian random sampling

# Cartesian random sampling

**Advantages** of Cartesian random sampling patterns:

- Easy to implement: standard FFT/gradients + binary mask
- Incoherent aliasing artifacts
- Allows non-uniform sampling by non-uniform probability for sampling points

**Open question:** Good choice for non-uniform probability (how to sample middle frequencies?)

**Idea:** look at coefficient distribution of (reasonably similar) template images (only magnitude important, not phase!)

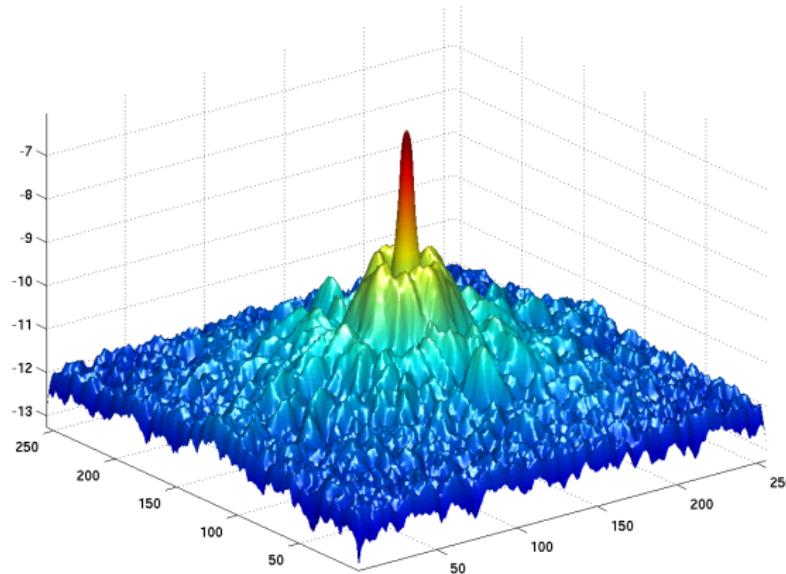
# Adapted Cartesian random sampling

## Procedure

- 1: choose template image  $u_t$  (same anatom. region, resolution)
- 2: set  $p = |\mathcal{F}u_t|$ , (apply smoothing/averaging,) rescale
- 3: **repeat**
- 4:     draw sampling points from Cartesian grid points using  
        Monte Carlo method with p.d.f.  $p$
- 5: **until** desired acceleration factor is reached
- 6: (add postprocessing to avoid holes)

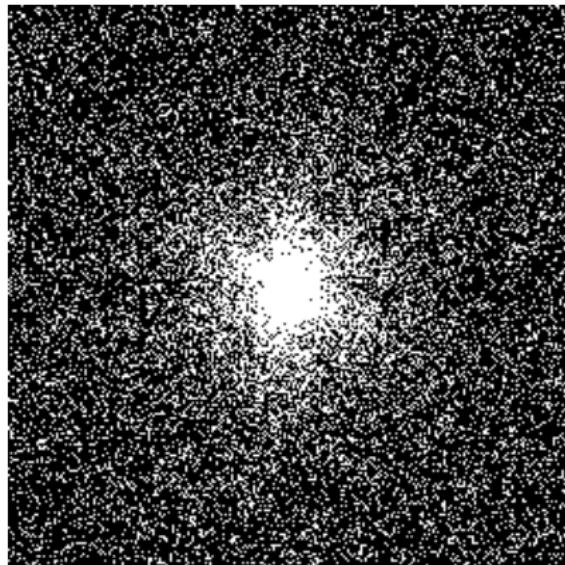
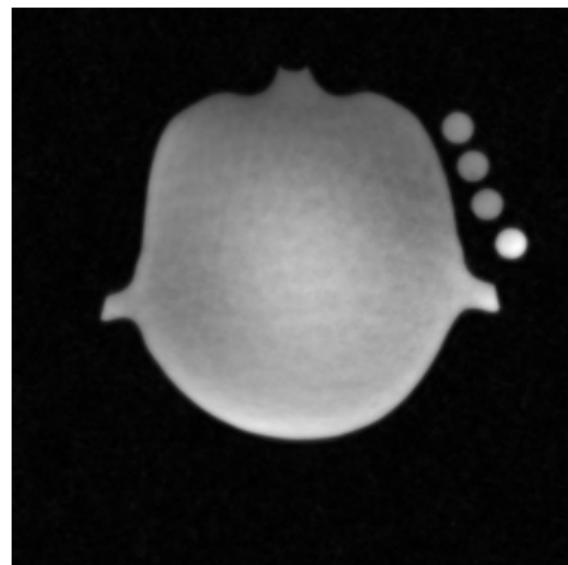
**Main advantage:** Good results without parameter tuning, robust

# Adapted random sampling: Example



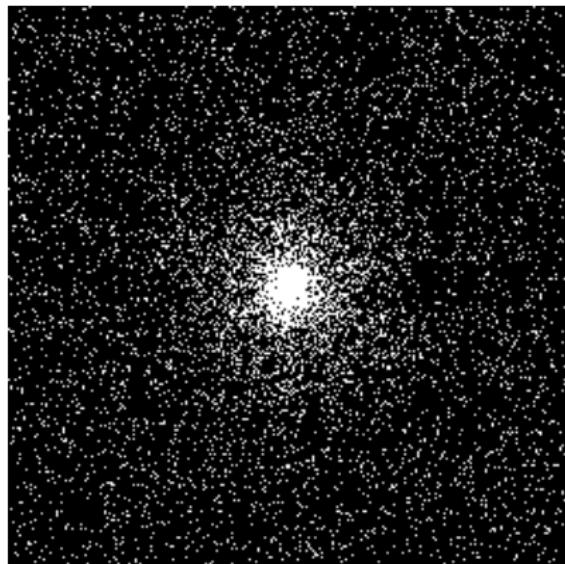
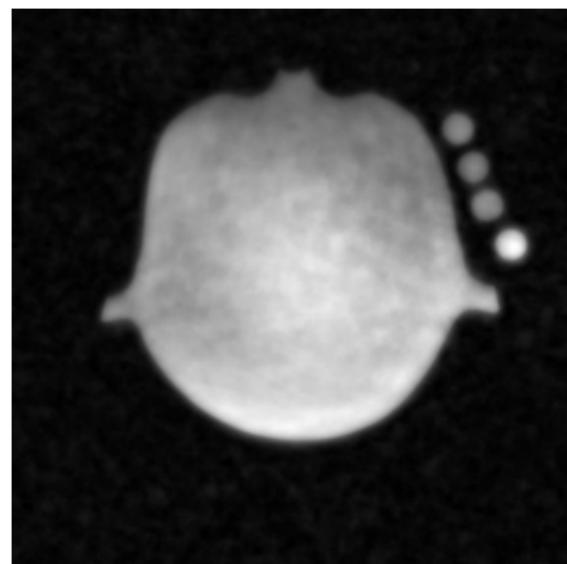
log-plot of probability density function (generated from raw data)

# Adapted random sampling: Example

(a) pattern  $R = 4$ 

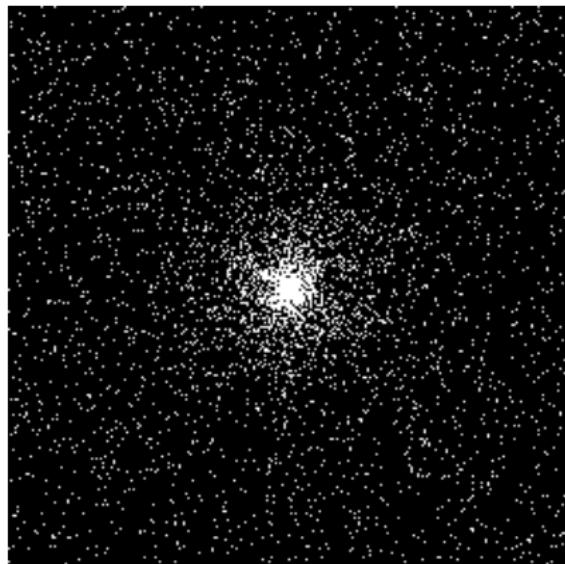
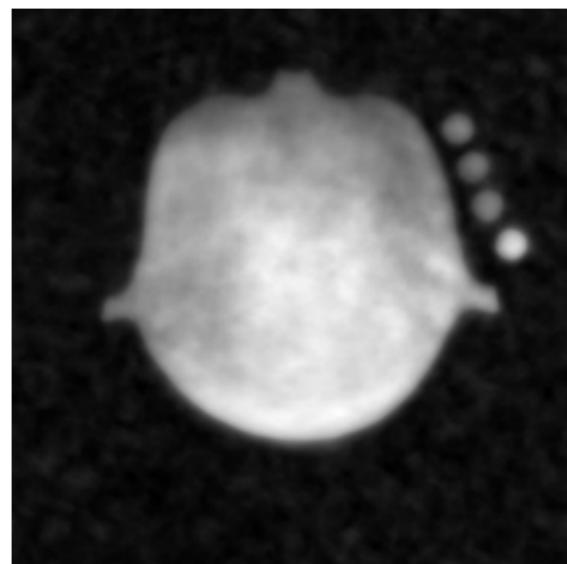
(b) zero-filled SOS (no dens. comp.)

# Adapted random sampling: Example

(c) pattern  $R = 10$ 

(d) zero-filled SOS (no dens. comp.)

# Adapted random sampling: Example

(e) pattern  $R = 18$ 

(f) zero-filled SOS (no dens. comp.)

# Choice of penalty

- IRGN suffers from noise amplification when  $\alpha_k$  too small
  - aliasing artifacts are incoherent, noise-like
- ~~~ add stronger penalty for image content

Here:

Total variation

$$TV(u) = \int |\nabla u|_2 dx$$

Pro: preserves edges while removing smooth variations

Con: non-quadratic, non-differentiable

## IRGNTV

Replace  $L^2$  penalty on  $u^{k+1}$  with  $TV$ :

- 1: Choose  $x^0 = (u^0, c^0)$ ,  $\alpha_0, \beta_0, q < 1$
- 2: **repeat**
- 3:     Solve for  $\delta x = (\delta u, \delta c)$

$$\begin{aligned} \min_{\delta x} \frac{1}{2} \|F'(x^k)\delta x + F(x^k) - g\|^2 + \frac{\alpha_k}{2} \|W(c^k + \delta c)\|^2 \\ + \beta_k TV(u^k + \delta u) \end{aligned}$$

- 4:     Set  $x^{k+1} = x^k + \delta x$ ,  $\alpha_{k+1} = \alpha_k q$ ,  $\beta_{k+1} = \beta_k q$ ,  $k = k + 1$
- 5: **until**  $\|F(x^k) - g\| < tol$
- 6: **return**  $u, c$

# Solution of TV subproblems

Set  $J(\delta x) := \frac{1}{2} \|F'(x^k)\delta x + F(x^k) - g\|^2 + \frac{\alpha_k}{2} \|W(c^k + \delta c)\|^2$

## Step 3

$$\min_{\delta u, \delta c} J(\delta u, \delta c) + \beta_k TV(u^k + \delta u)$$

**non-smooth, convex** optimization problem  $\rightsquigarrow$  use **convex duality**

$$\beta TV(u) = \sup_{\{|p(x)|_2 \leq \beta\}} \langle u, -\operatorname{div} p \rangle$$

# Solution of TV subproblems

## Saddle point problem

$$\min_{\delta u, \delta c} \max_{p \in C_{\beta_k}} J(\delta u, \delta c) + \langle u^k + \delta u, -\operatorname{div} p \rangle$$

with  $C_\beta = \{p : |p(x)|_2 \leq \beta \text{ for all } x\}$  convex,  $J$  differentiable

~~> use **projected gradient descent/ascent method**:

- Requires only application of  $F'$ ,  $F'^*$  (i.e.,  $\mathcal{F}_s$ ,  $\mathcal{F}_s^*$ )
- Straightforward parallelization
- Order-optimal algorithms available

Here: **Primal-dual extragradient algorithm**, based on  
*Pock/Cremers/Bischof/Chambolle (2009)*

# Primal-dual extragradient method

```
1: function TVSOLVE( $u, c, \alpha, \beta, \sigma_u, \sigma_c, \tau$ )
2:    $\delta u, \bar{\delta u}, \delta c, \bar{\delta c}, p \leftarrow 0$ 
3:   repeat
4:      $p \leftarrow \text{proj}_{\beta}(p + \tau \nabla(u + \bar{\delta u}))$ 
5:      $\delta u_{old} \leftarrow \delta u, \delta c_{old} \leftarrow \delta c$ 
6:      $\delta u \leftarrow \delta u - \sigma_u(\partial_u J(u, c)(\bar{\delta u}, \bar{\delta c}) - \text{div } p)$ 
7:      $\delta c \leftarrow \delta c - \sigma_c(\partial_c J(u, c)(\bar{\delta u}, \bar{\delta c}))$ 
8:      $\bar{\delta u} \leftarrow 2\delta u - \delta u_{old}$ 
9:      $\bar{\delta c} \leftarrow 2\delta c - \delta c_{old}$ 
10:    until convergence
11:    return  $\delta u, \delta c$ 
12: end function
```

# Algorithm

- Compute projection on  $C_\beta$  pointwise by

$$\text{proj}_\beta(q)(x) = \frac{q(x)}{\max(1, \beta^{-1}|q(x)|_2)}$$

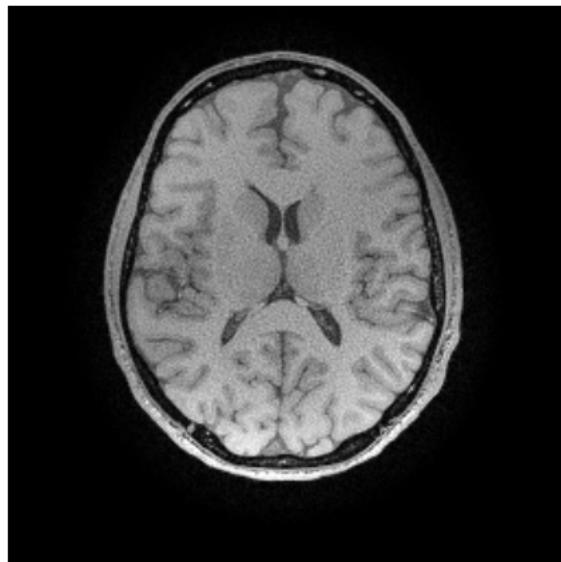
- Computation of  $\partial_u J(u, c)(\bar{\delta u}, \bar{\delta c})$  and  $\partial_c J(u, c)(\bar{\delta u}, \bar{\delta c})$  identical to CG iteration for IRGN
- Step lengths  $\sigma_u, \sigma_c, \tau$  related to Lipschitz constants of  $F'(u^k, c^k), \nabla$

► details

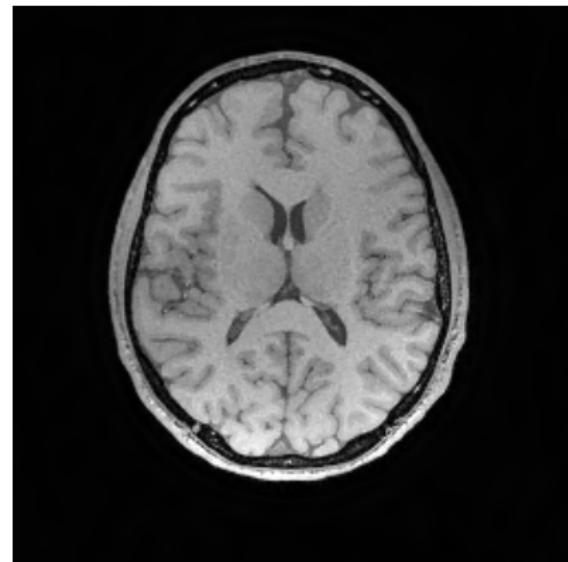
# Examples: random sampling

- raw data from brain and phantom
- 3D gradient echo sequence, 3T system, 12 channel head coil
- 8 (phantom: 9) virtual channels (SVD) used for reconstruction
- sequence modified using binary 2D mask to define subsampling pattern
- subsampling  $R = 4$  (10)
- sequence parameters
  - repetition time TR=20ms
  - echo time TE=5ms
  - flip angle FA= $18^\circ$
  - matrix size (x,y,z)=256x256x256
  - FOV=250mm
  - slice thickness brain 1mm (phantom 5mm)

# Reconstructions: random ( $R = 4$ )

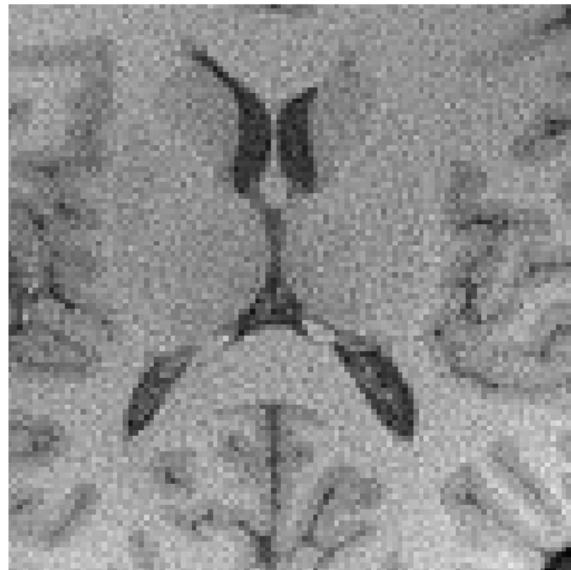


(a) IRGN



(b) IRGNTV

# Reconstructions: random ( $R = 4$ )

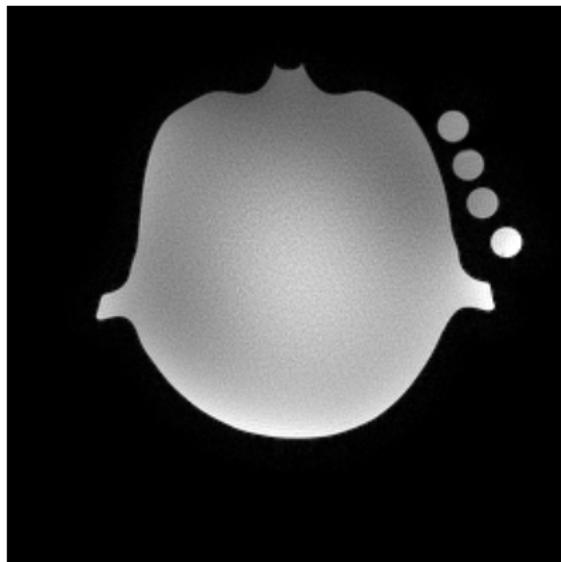


(a) IRGN (detail)

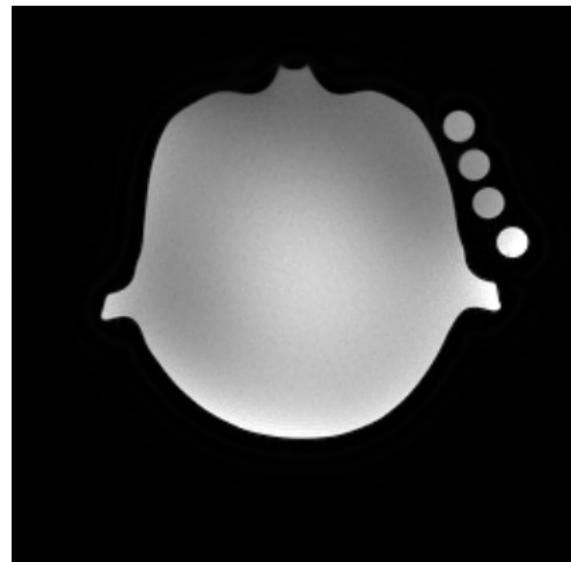


(b) IRGNTV (detail)

# Reconstructions: random ( $R = 4$ )



(a) IRGN



(b) IRGNTV

# Effect of TV

Since  $\beta_k \rightarrow 0$ , final TV effect is not very strong

**Pro:** No introduction of typical TV-artifacts (cartooning, stair-casing)

**Con:** Strong effect can be desired if piecewise constant is a good prior (i.e., for higher acceleration, cf. phantom)

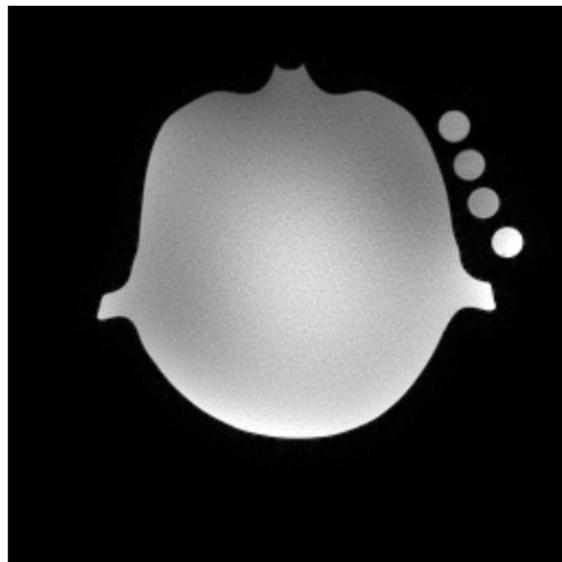
~~ stop decreasing TV penalty parameter at desired value:

$$\alpha_{k+1} = \alpha_k q$$

$$\beta_{k+1} = \max(\beta_{\min}, \beta_k q)$$

For illustration: Phantom with  $\beta_{\min} = 5 \cdot 10^{-3}$

# Effect of TV ( $R = 4$ )

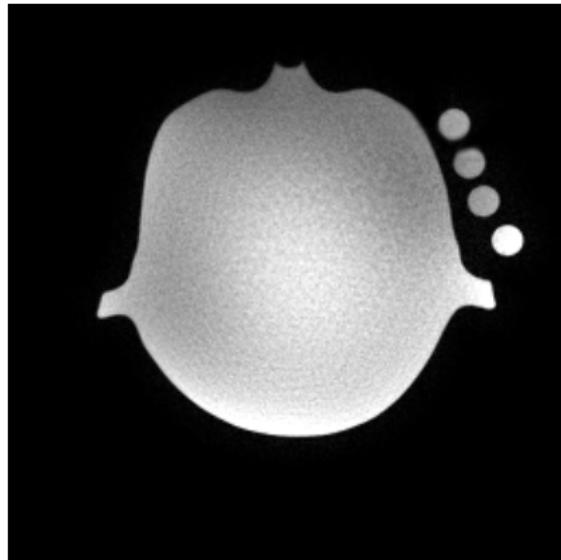


(a) IRGN

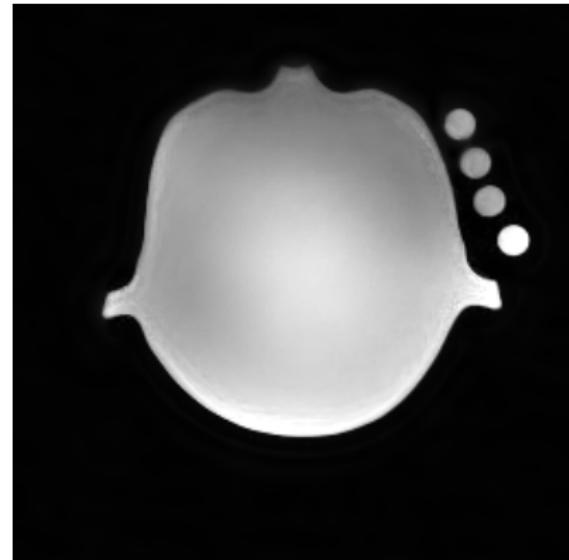


(b) IRGNTV

# Effect of TV ( $R = 10$ )



(a) IRGN



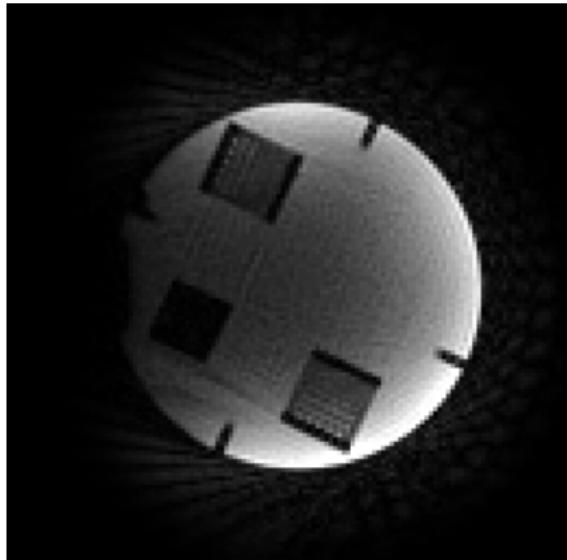
(b) IRGNTV

# Examples: radial sampling

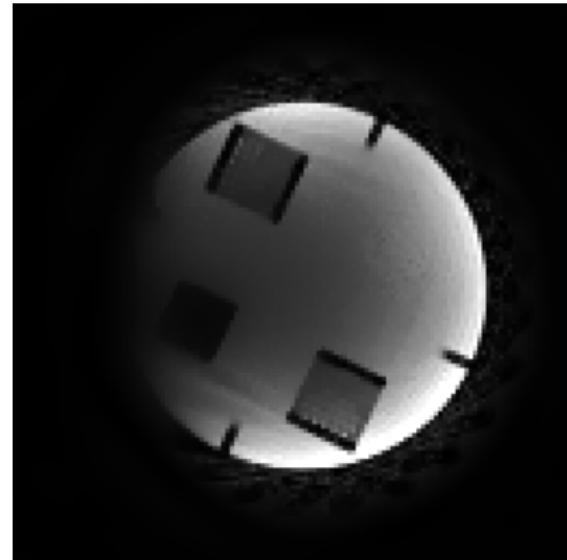
- raw data of phantom and heart
- radial FLASH sequence, 3T System, 32 channel coil
- 8 (cardiac: 12) virtual channels (SVD) used for reconstruction
- 25 (19) projections,  $R \approx 8$  (10.5)
- **No postprocessing, temporal view sharing**
- sequence parameters
  - repetition time TR=2.0ms
  - echo time TE=1.3ms
  - flip angle FA=8°
  - 256 points per proj. (2x oversampling)  $\leadsto$  matrix 128x128
  - slice thickness 8mm, in plane resolution 2mm x 2mm

(data courtesy of Martin Uecker)

# Radial sampling: phantom (25 proj)

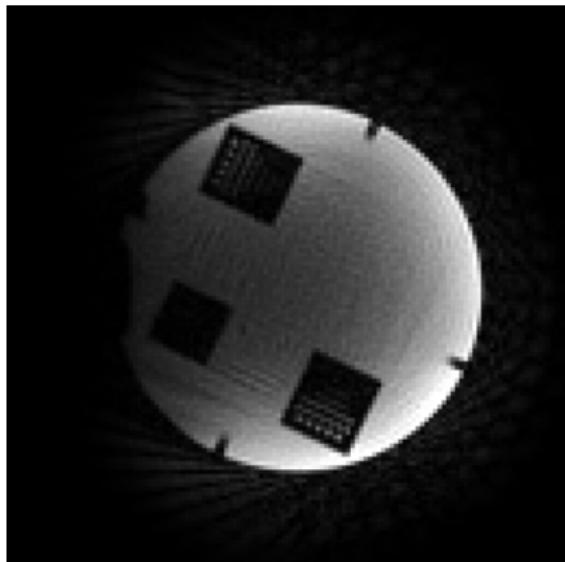


(a) IRGN

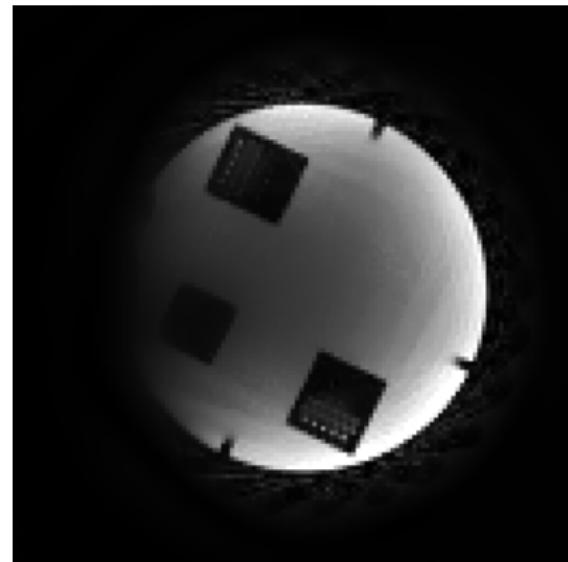


(b) IRGNTV

# Radial sampling: phantom (25 proj)

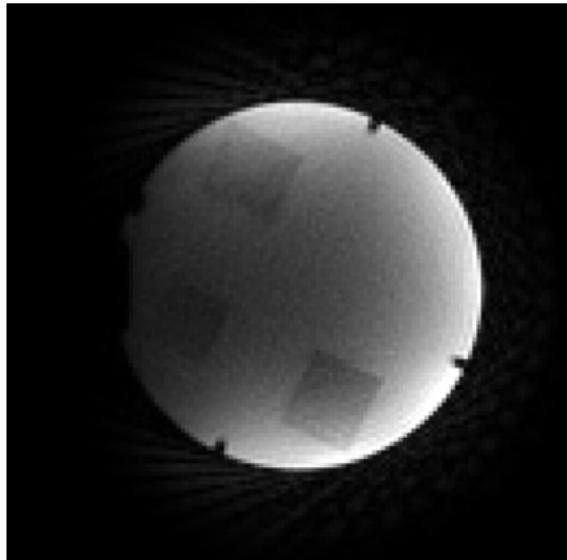


(a) IRGN

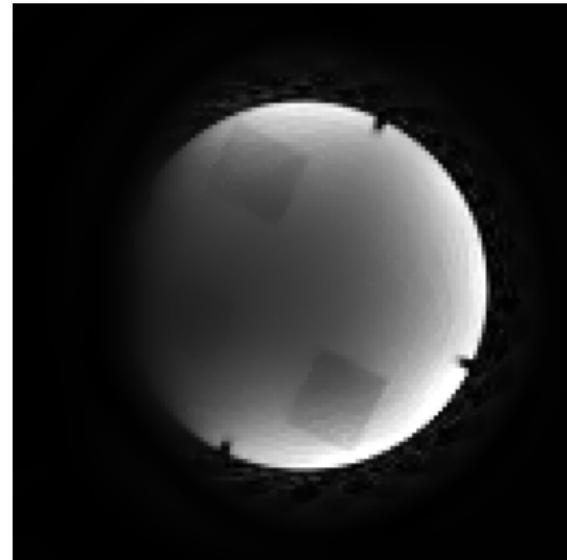


(b) IRGNTV

# Radial sampling: phantom (25 proj)

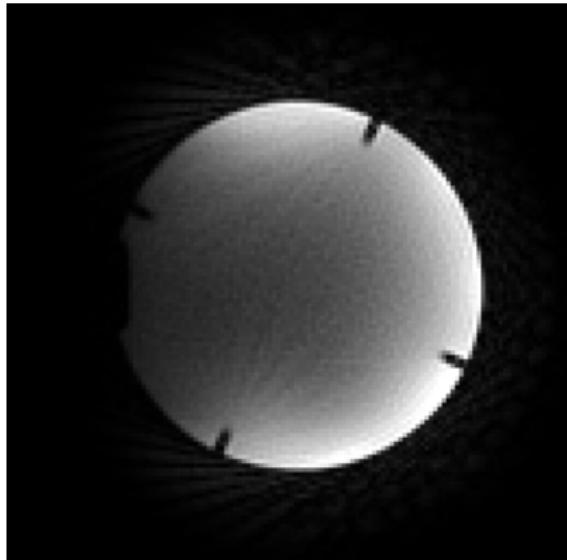


(a) IRGN

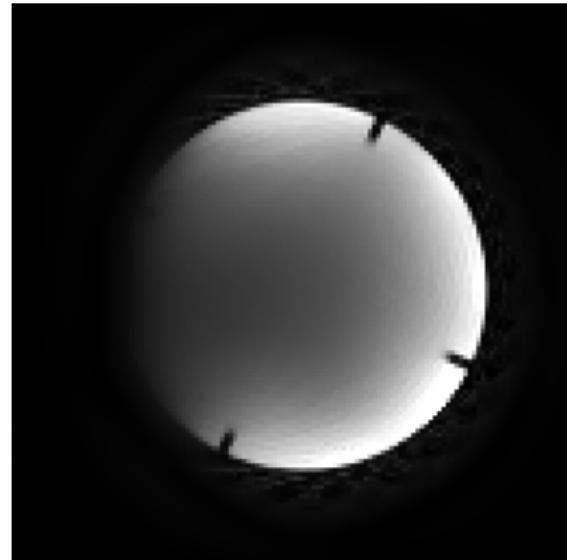


(b) IRGNTV

# Radial sampling: phantom (25 proj)

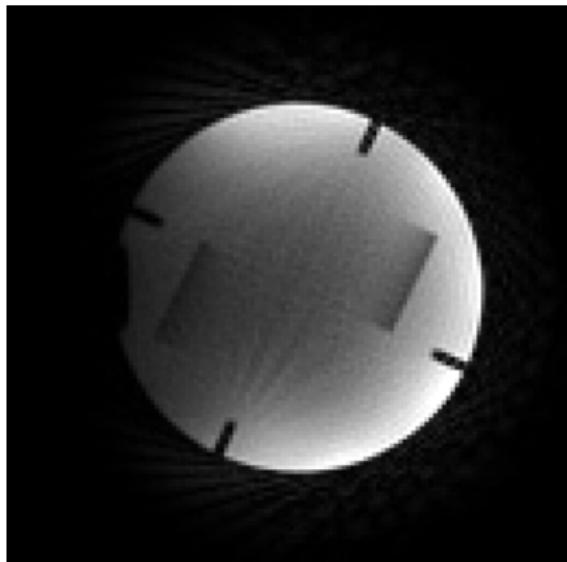


(a) IRGN

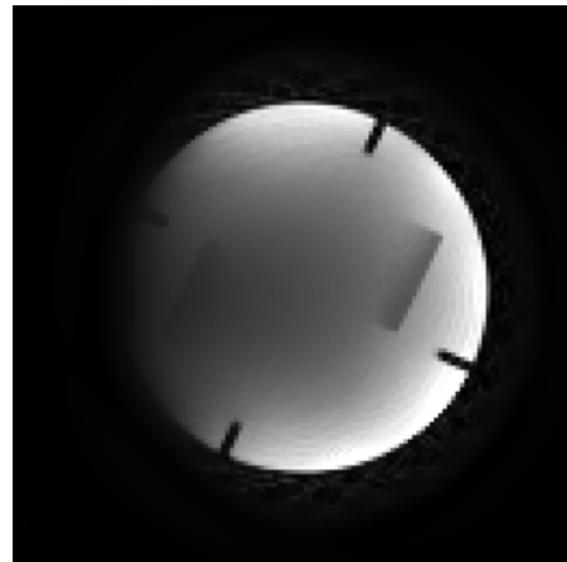


(b) IRGNTV

# Radial sampling: phantom (25 proj)

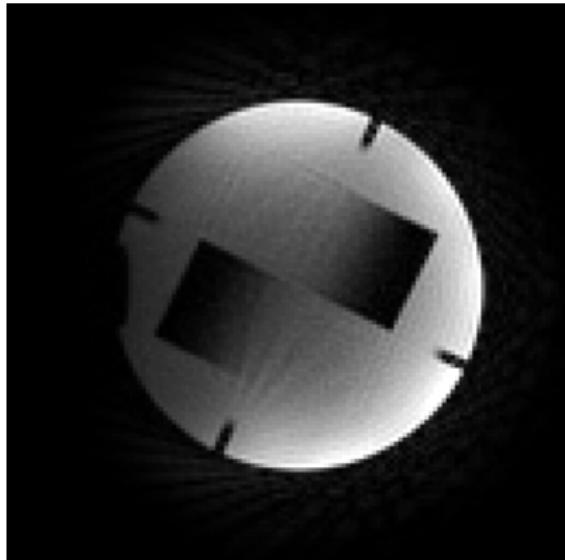


(a) IRGN

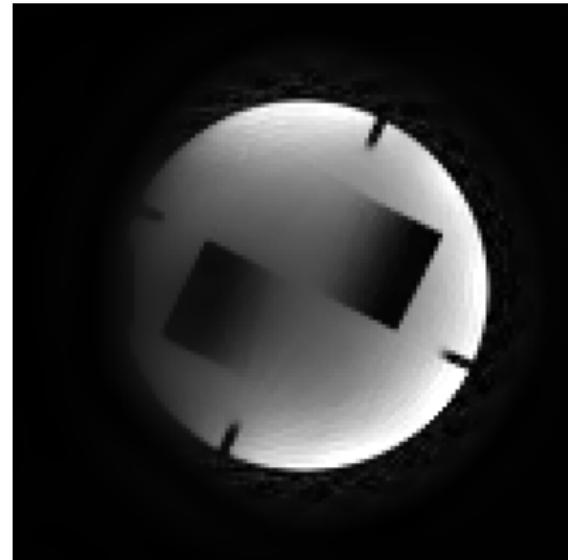


(b) IRGNTV

# Radial sampling: phantom (25 proj)

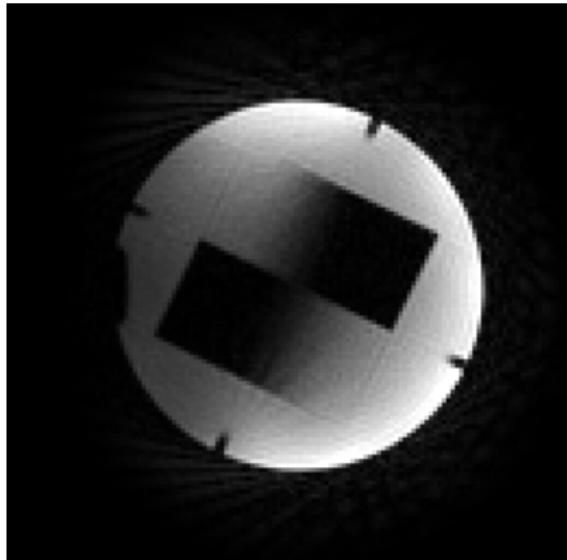


(a) IRGN

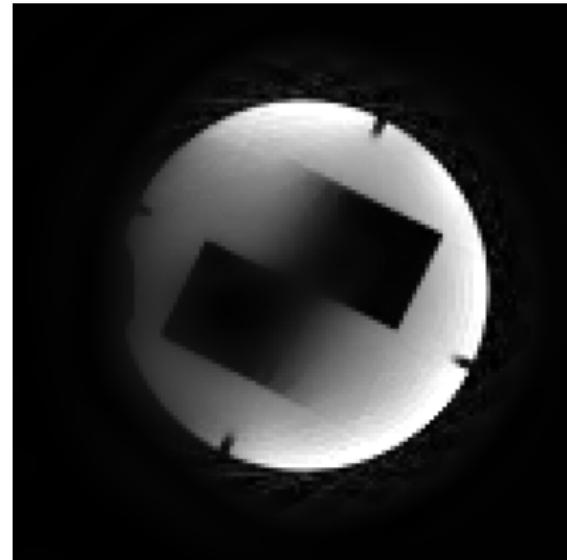


(b) IRGNTV

# Radial sampling: phantom (25 proj)

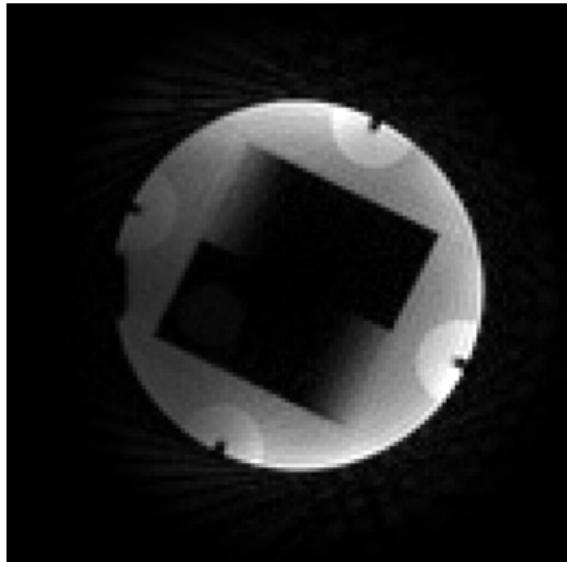


(a) IRGN

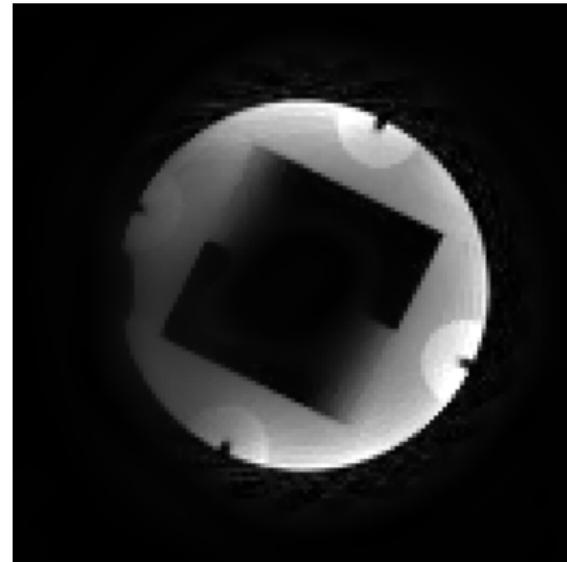


(b) IRGNTV

# Radial sampling: phantom (25 proj)

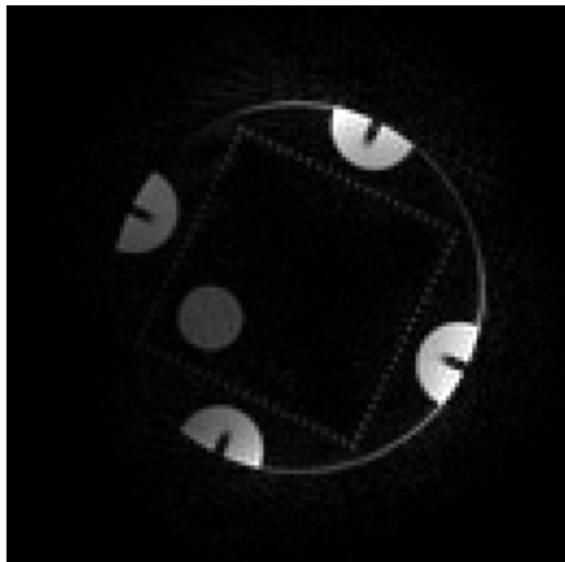


(a) IRGN

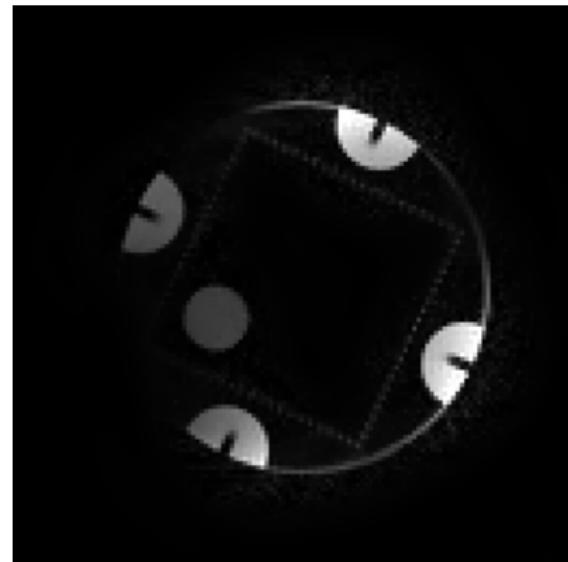


(b) IRGNTV

# Radial sampling: phantom (25 proj)

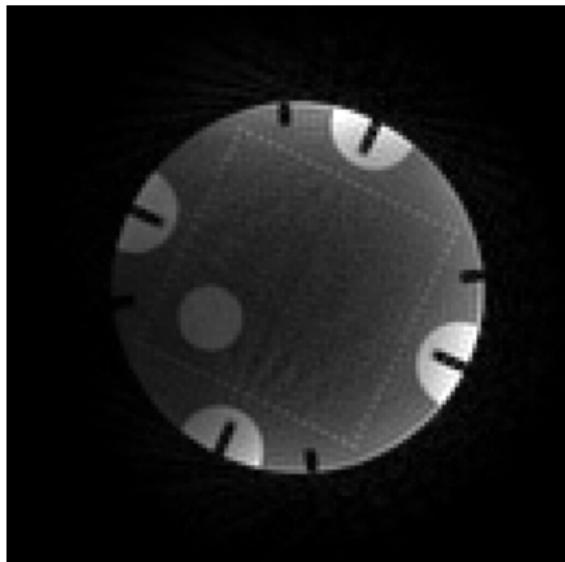


(a) IRGN

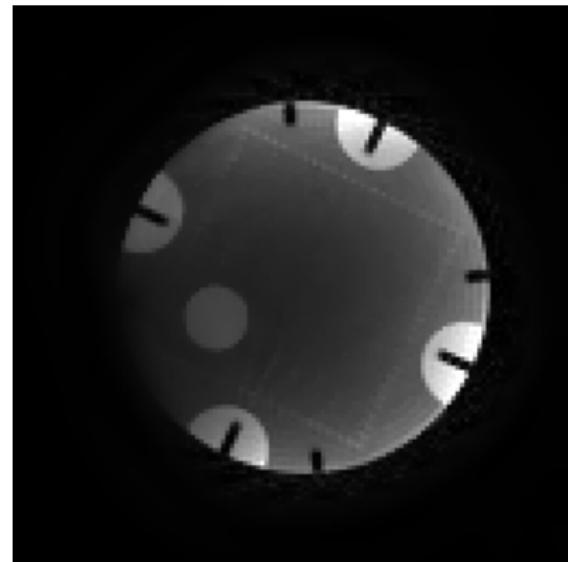


(b) IRGNTV

# Radial sampling: phantom (25 proj)

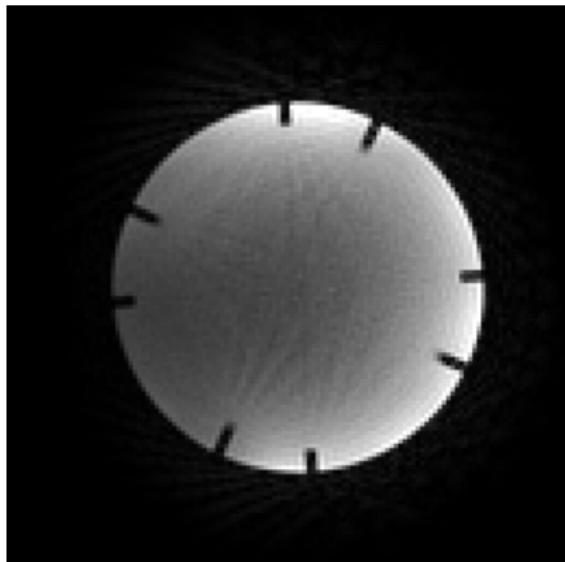


(a) IRGN

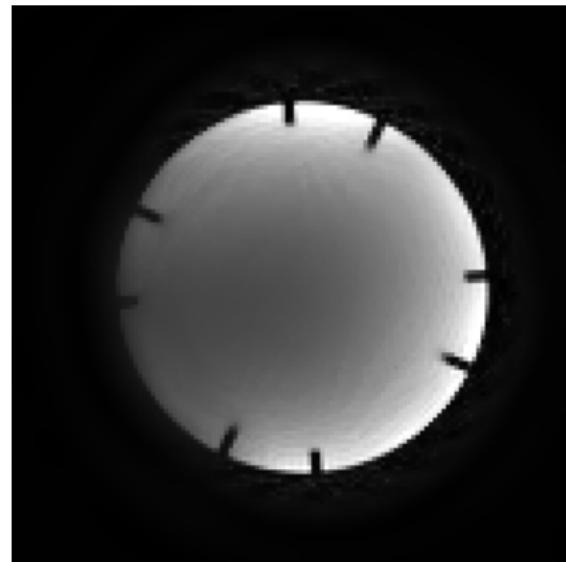


(b) IRGNTV

# Radial sampling: phantom (25 proj)

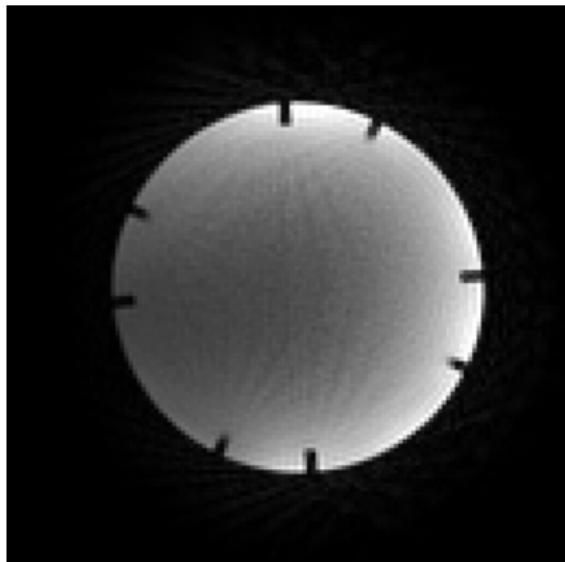


(a) IRGN

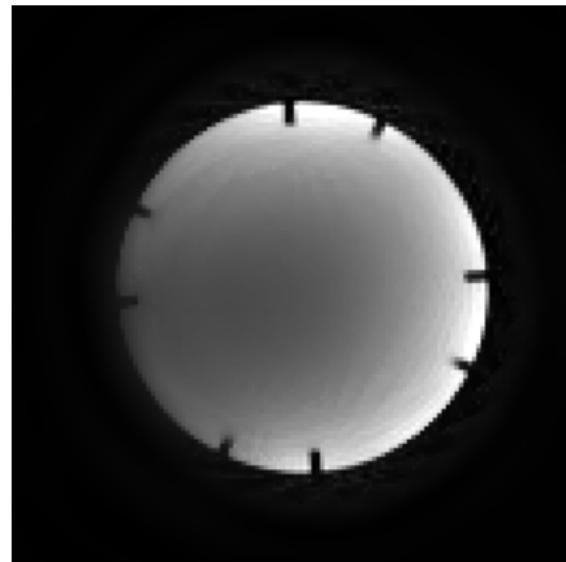


(b) IRGNTV

# Radial sampling: phantom (25 proj)

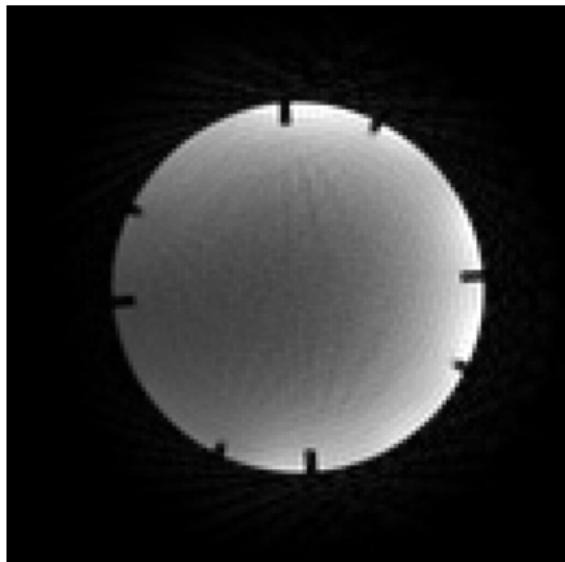


(a) IRGN

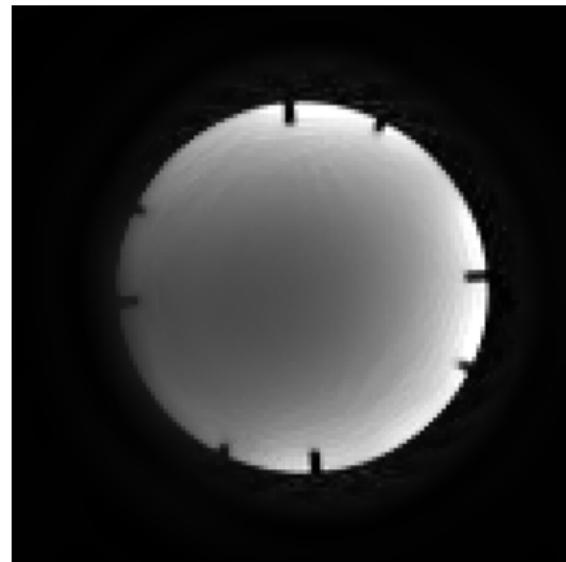


(b) IRGNTV

# Radial sampling: phantom (25 proj)

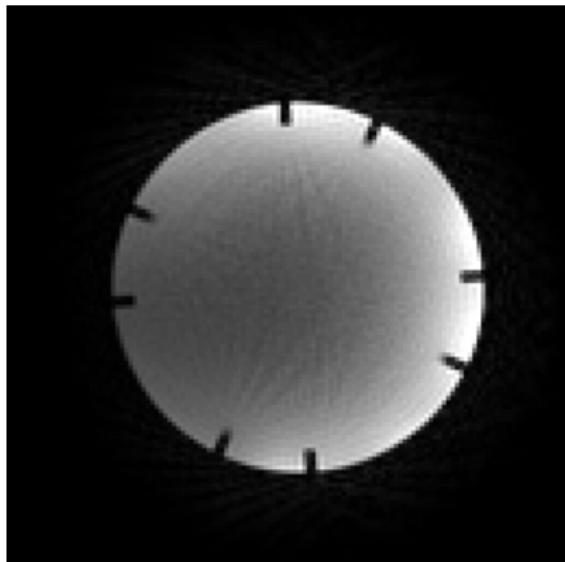


(a) IRGN

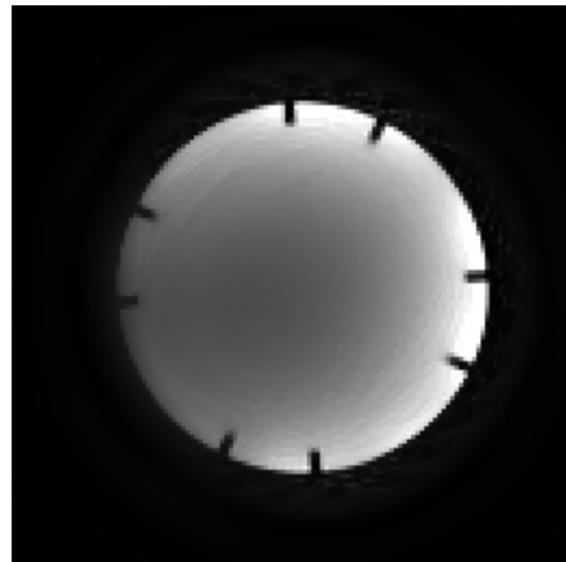


(b) IRGNTV

# Radial sampling: phantom (25 proj)

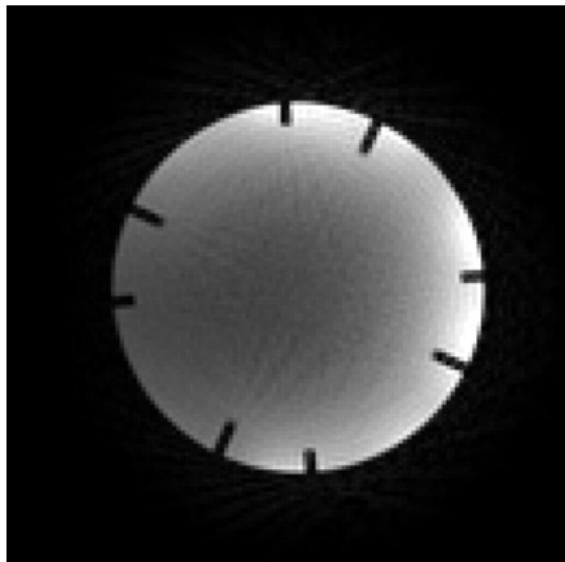


(a) IRGN

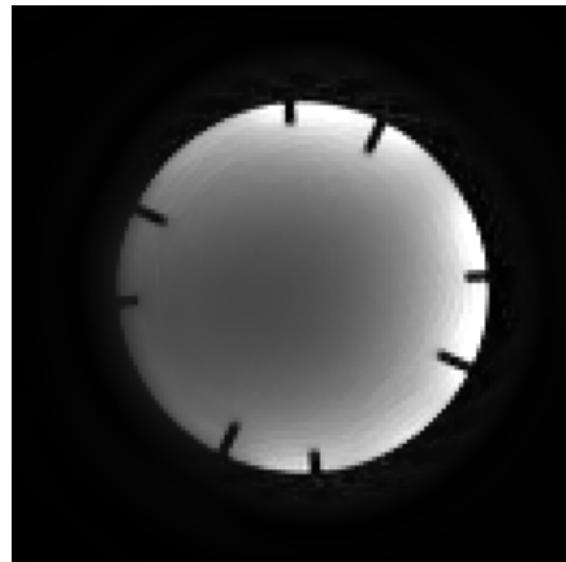


(b) IRGNTV

# Radial sampling: phantom (25 proj)

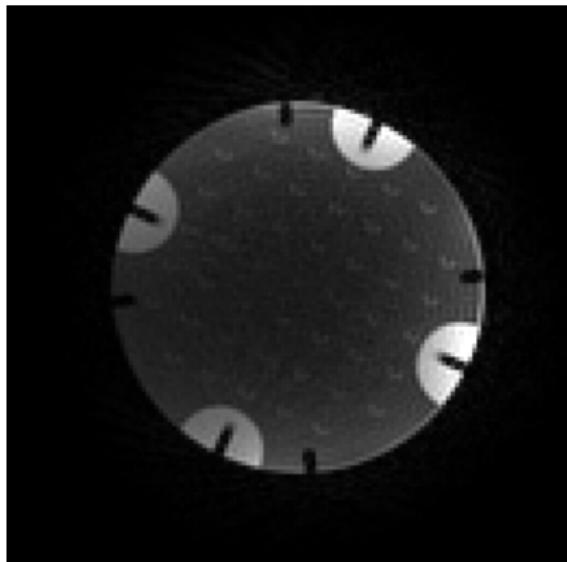


(a) IRGN

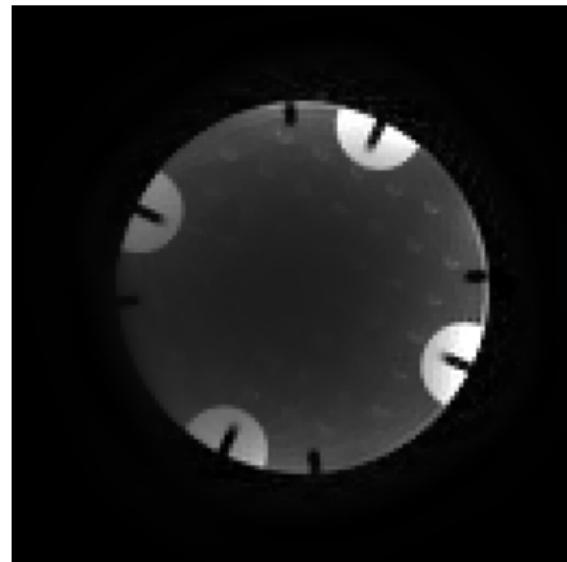


(b) IRGNTV

# Radial sampling: phantom (25 proj)

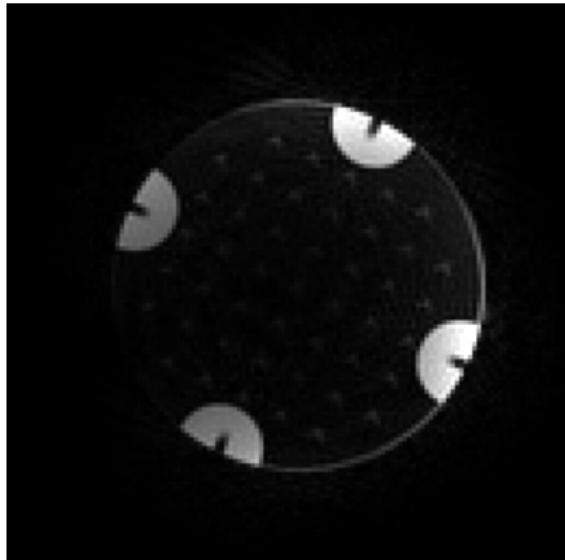


(a) IRGN

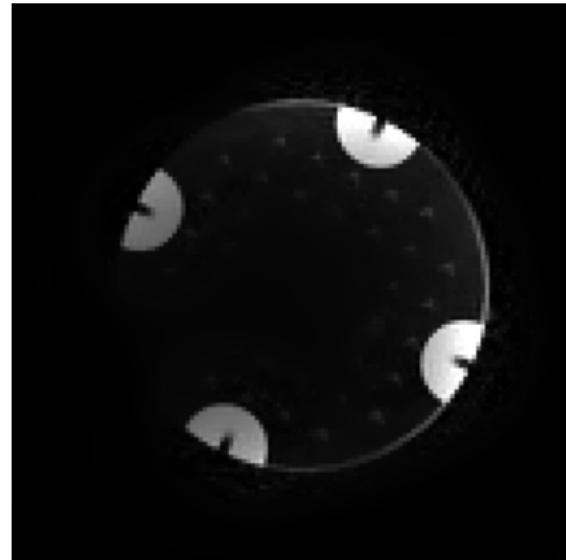


(b) IRGNTV

# Radial sampling: phantom (25 proj)

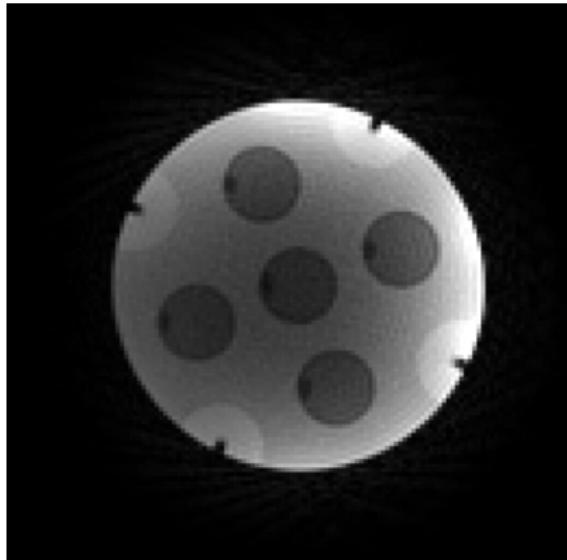


(a) IRGN

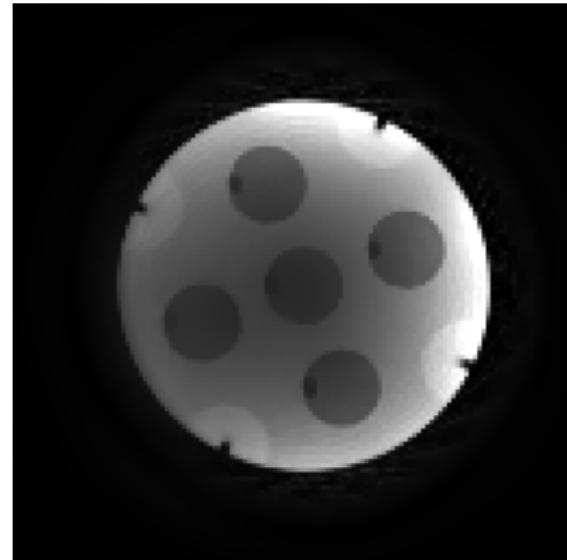


(b) IRGNTV

# Radial sampling: phantom (25 proj)

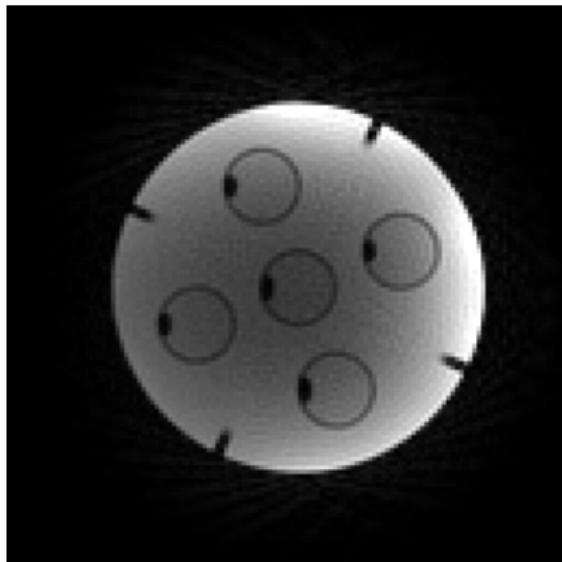


(a) IRGN

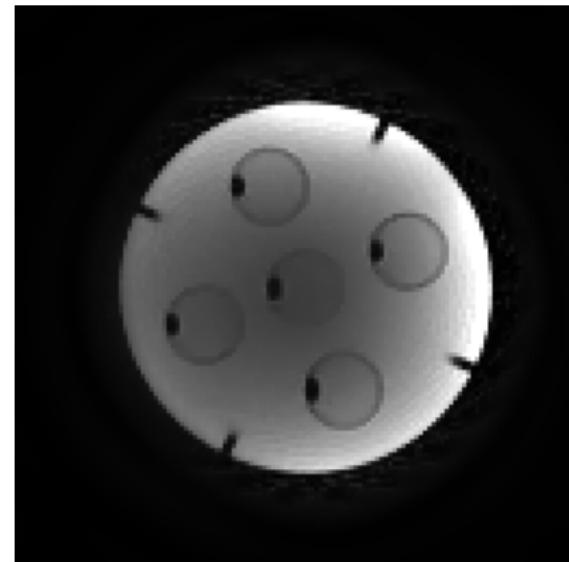


(b) IRGNTV

# Radial sampling: phantom (25 proj)

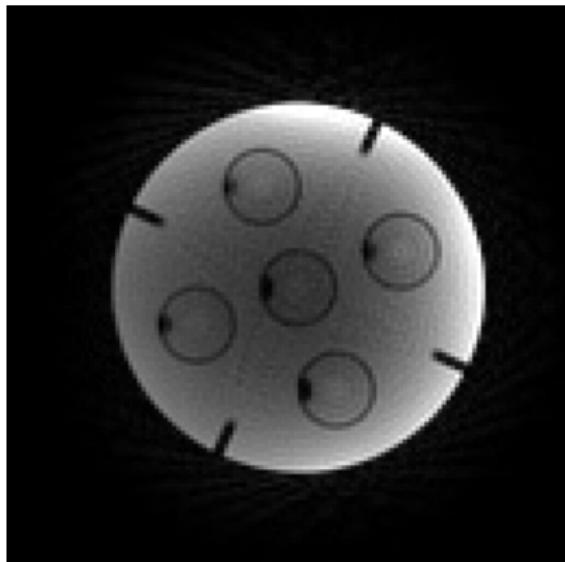


(a) IRGN

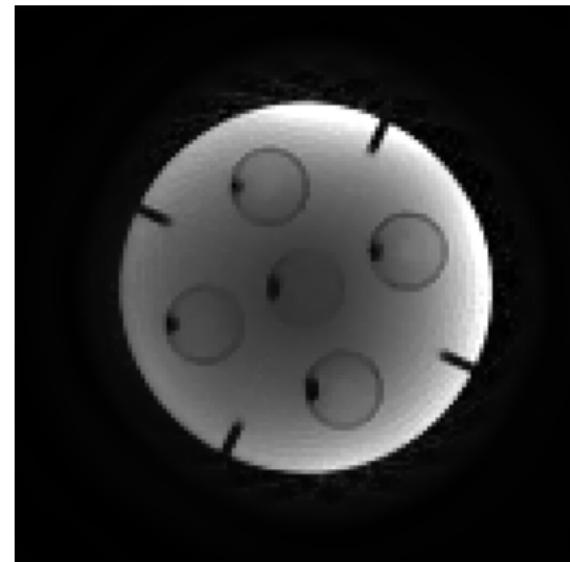


(b) IRGNTV

# Radial sampling: phantom (25 proj)

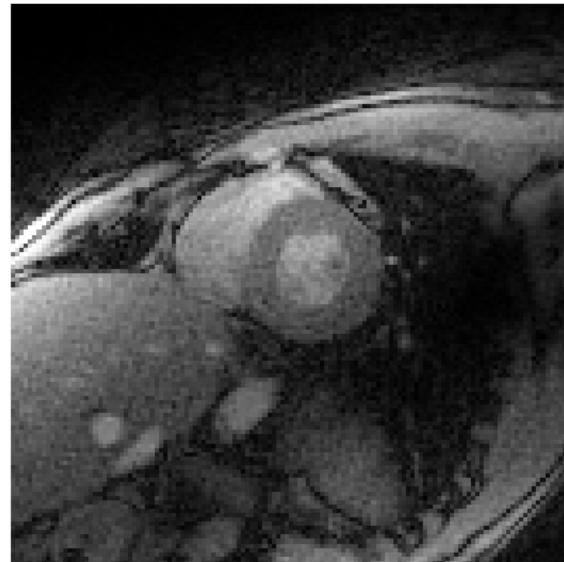


(a) IRGN

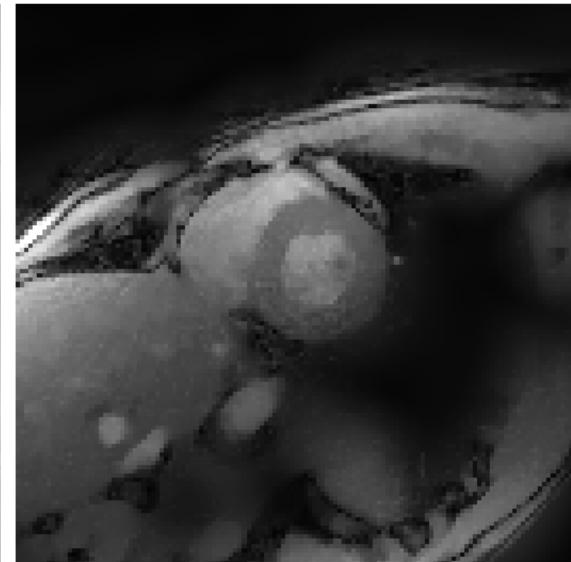


(b) IRGNTV

# Radial sampling: cardiac (25 proj $\approx$ 20 fps)

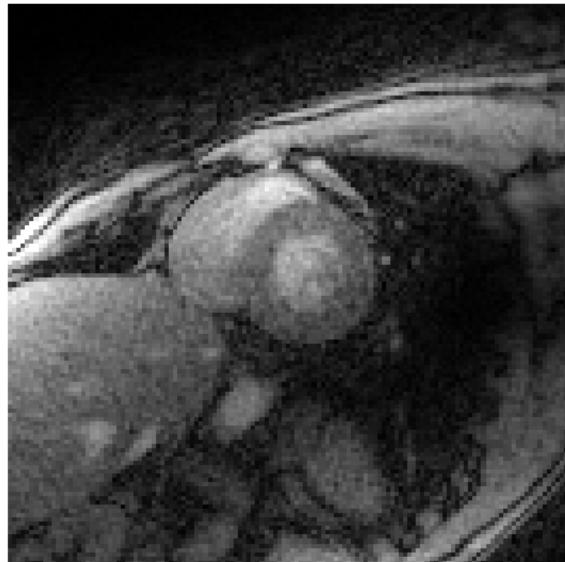


(a) IRGN

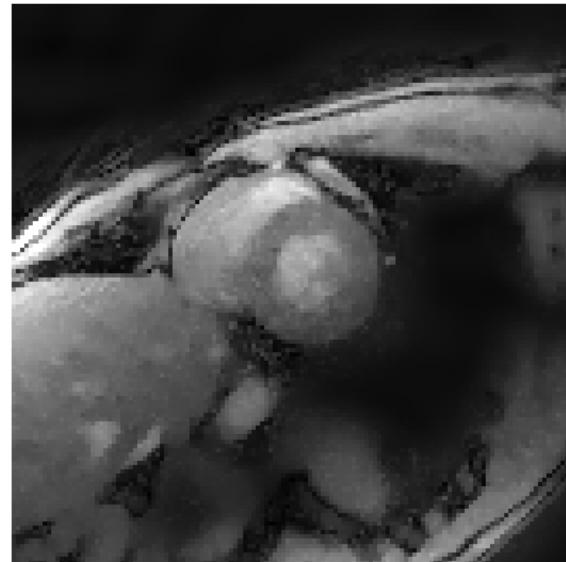


(b) IRGNTV

# Radial sampling: cardiac (19 proj $\approx$ 26 fps)



(a) IRGN



(b) IRGNTV

# Total generalized variation (TGV)

Large TV penalty leads to stair-casing  $\rightsquigarrow$  include penalty on higher derivatives, promoting piecewise smooth reconstruction

Here: second order **total generalized variation**

$$\beta TGV^2(u) = \sup_{v \in C_\beta^2} \langle u, \operatorname{div}^2 v \rangle$$

with

$$C_\beta^2 = \{v \in \mathcal{C}_c^2(\Omega, \mathcal{S}^{d \times d}) : \|v\|_\infty \leq 2\beta, \|\operatorname{div} v\|_\infty \leq \beta\}$$

(see <http://math.uni-graz.at/mobis/publications/SFB-Report-2010-023.pdf> for details)

# IRGNTGV

Replace  $TV$  penalty on  $u^{k+1}$  with  $TGV$ :

1: Choose  $x^0 = (u^0, c^0)$ ,  $\alpha_0, \beta_0, q < 1$

2: **repeat**

3:     Solve for  $\delta x = (\delta u, \delta c)$

$$\begin{aligned} \min_{\delta x} \frac{1}{2} \|F'(x^k)\delta x + F(x^k) - g\|^2 + \frac{\alpha_k}{2} \|W(c^k + \delta c)\|^2 \\ + \beta_k TGV^2(u^k + \delta u) \end{aligned}$$

4:     Set  $x^{k+1} = x^k + \delta x$ ,  $\alpha_{k+1} = \alpha_k q$ ,  $\beta_{k+1} = \beta_k q$ ,  $k = k + 1$

5: **until**  $\|F(x^k) - g\| < tol$

6: **return**  $u, c$

# Solution of IRGNTGV subproblems

Convex duality:

$$\beta TGV^2(u) = \inf_v \beta \|\nabla u - v\| + 2\beta \|\mathcal{E}v\|$$

Here:  $v \in \mathcal{C}^1(\Omega, \mathbb{C}^d)$ ,  $\mathcal{E}v = \frac{1}{2}(\nabla v + \nabla v^T) = (-\operatorname{div}^2)^*v$

~ Interpretation: TGV balances first and second derivative

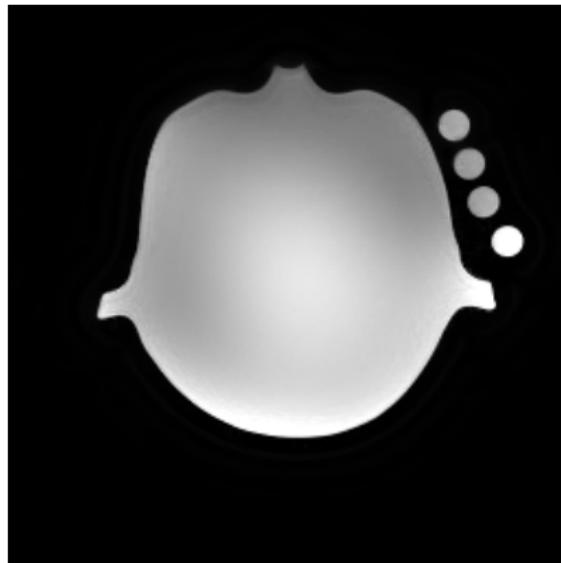
Saddle point problem

$$\min_{\delta u, \delta c, v} \max_{\substack{p \in C_{\beta_k} \\ q \in C_{2\beta_k}}} J(\delta u, \delta c) + \langle \nabla u^k + \delta u - v, p \rangle + \langle \mathcal{E}v, q \rangle$$

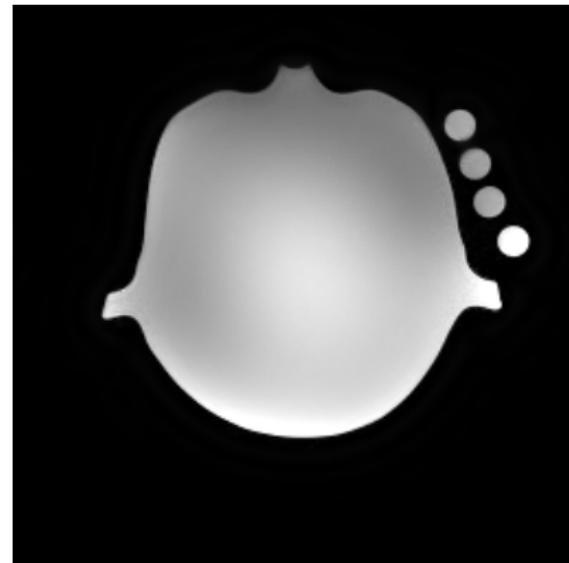
# Primal-dual extragradient method

```
1: function TGVOLVE( $u, c, \alpha, \beta, \sigma_u, \sigma_c, \sigma_v, \tau$ )
2:    $\delta u, \bar{\delta u}, \delta c, \bar{\delta c}, v, \bar{v}, p, q \leftarrow 0$ 
3:   repeat
4:      $p \leftarrow \text{proj}_{\beta}(p + \tau(\nabla(u + \bar{\delta u}) - v))$ 
5:      $q \leftarrow \text{proj}_{2\beta}(q + \tau(\mathcal{E}v))$ 
6:      $\delta u_{old} \leftarrow \delta u, \delta c_{old} \leftarrow \delta c, v_{old} \leftarrow v$ 
7:      $\delta u \leftarrow \delta u - \sigma_u(\partial_u J(u, c)(\bar{\delta u}, \bar{\delta c}) - \text{div } p)$ 
8:      $\delta c \leftarrow \delta c - \sigma_c(\partial_c J(u, c)(\bar{\delta u}, \bar{\delta c}))$ 
9:      $v \leftarrow v - \sigma_v(-p - \text{div}^2 q)$ 
10:     $\bar{\delta u} \leftarrow 2\delta u - \delta u_{old}$ 
11:     $\bar{\delta c} \leftarrow 2\delta c - \delta c_{old}$ 
12:     $\bar{v} \leftarrow 2v - v_{old}$ 
13:   until convergence
14: end function
```

# Effect of TGV: Random ( $R = 4$ )

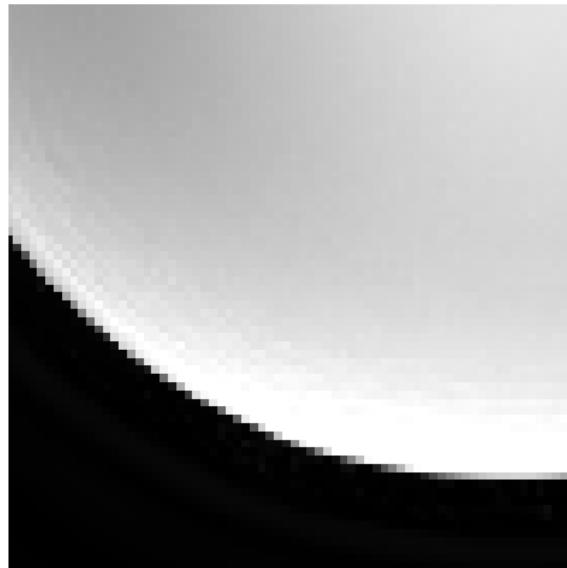


(a) IRGNTV

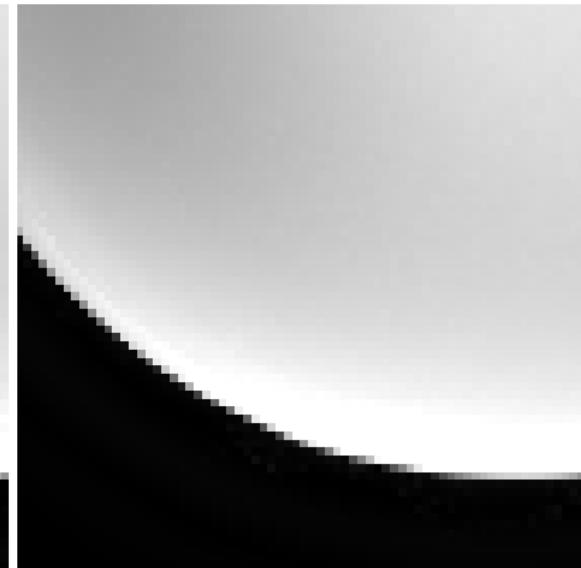


(b) IRGNTGV

# Effect of TGV: Random ( $R = 4$ )

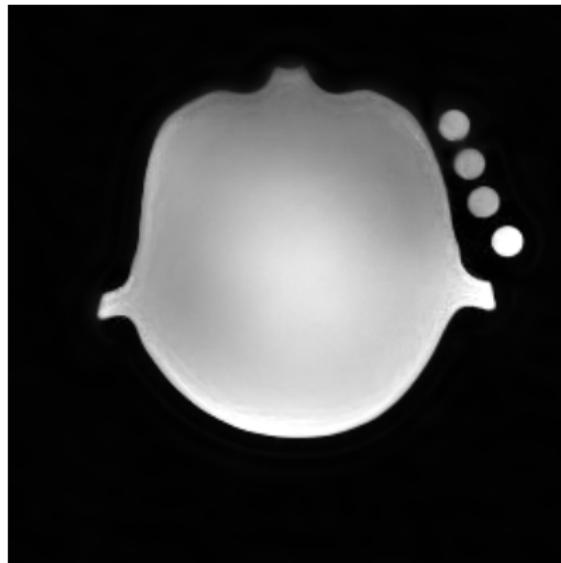


(a) IRGNTV (detail)

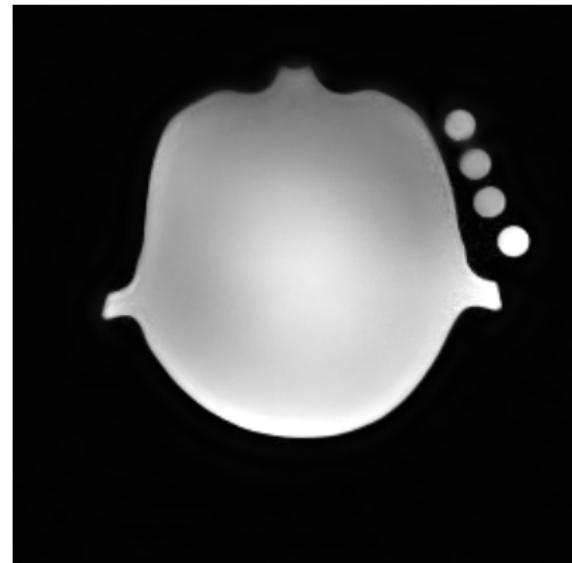


(b) IRGNTGV (detail)

# Effect of TGV: Random ( $R = 10$ )

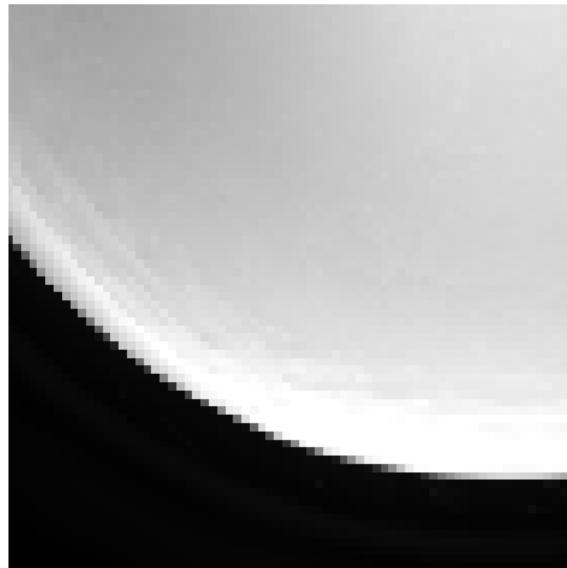


(a) IRGNTV

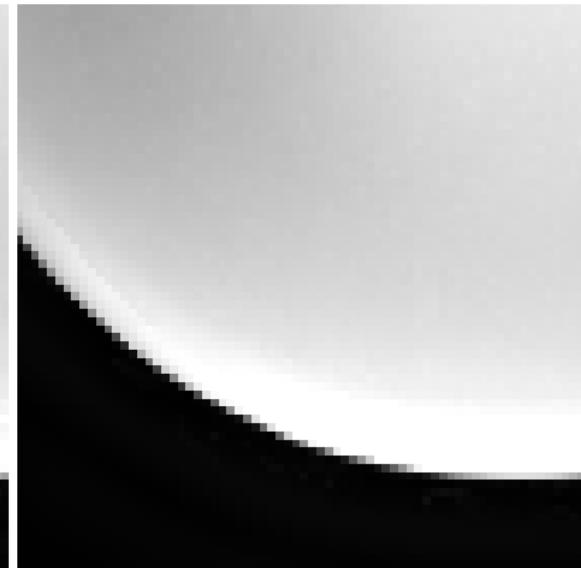


(b) IRGNTGV

# Effect of TGV: Random ( $R = 10$ )

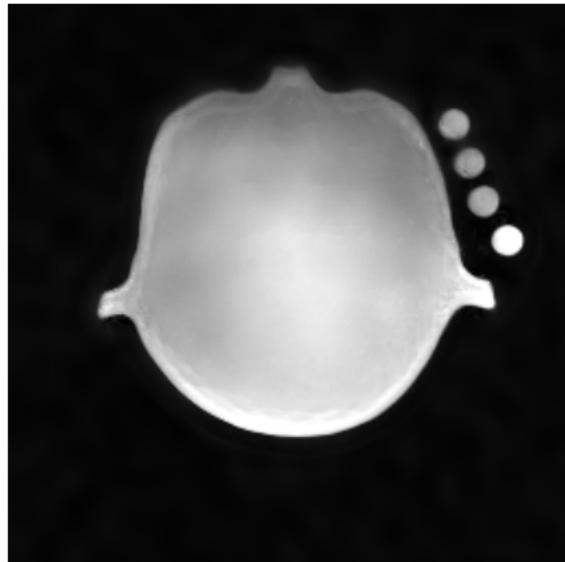


(a) IRGNTV (detail)

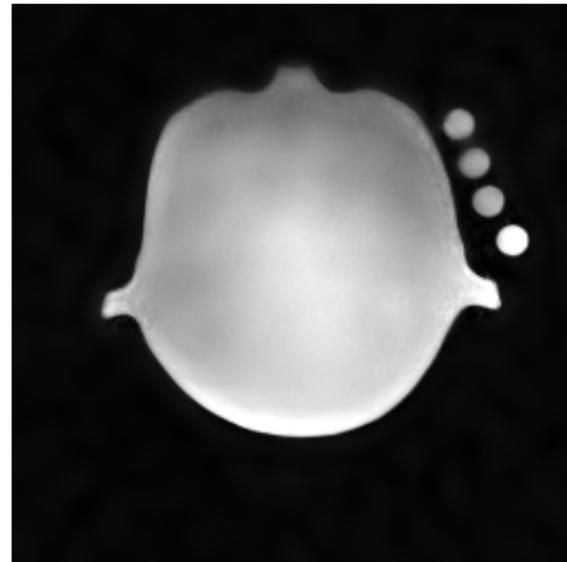


(b) IRGNTGV (detail)

# Effect of TGV: Random ( $R = 18$ )

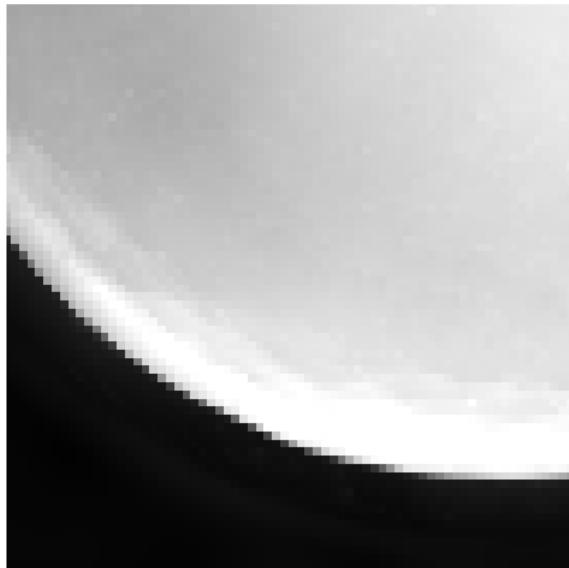


(a) IRGNTV

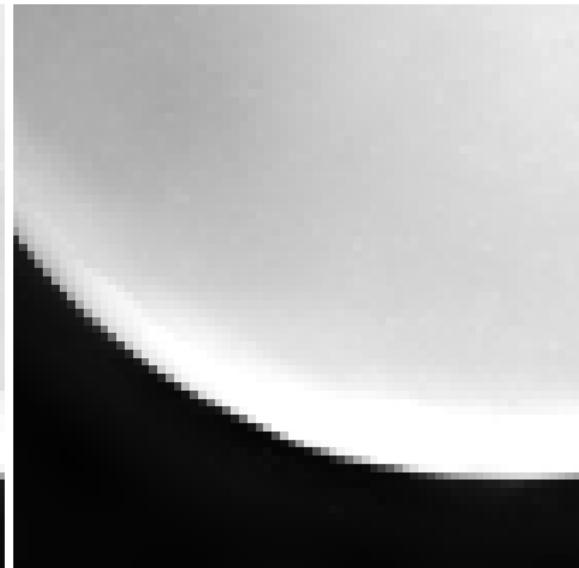


(b) IRGNTGV

# Effect of TGV: Random ( $R = 18$ )

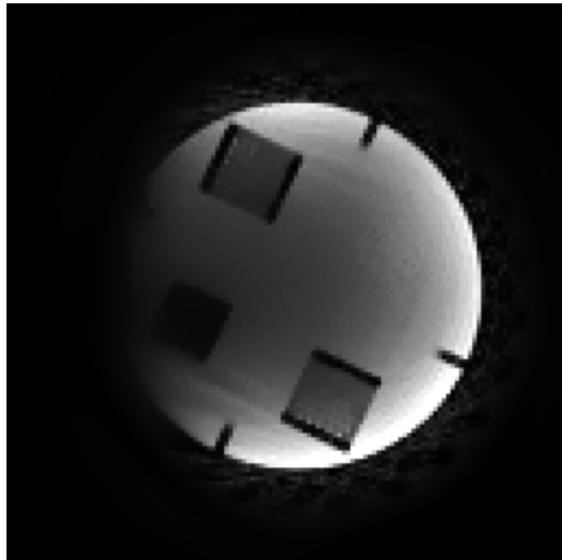


(a) IRGNTV (detail)

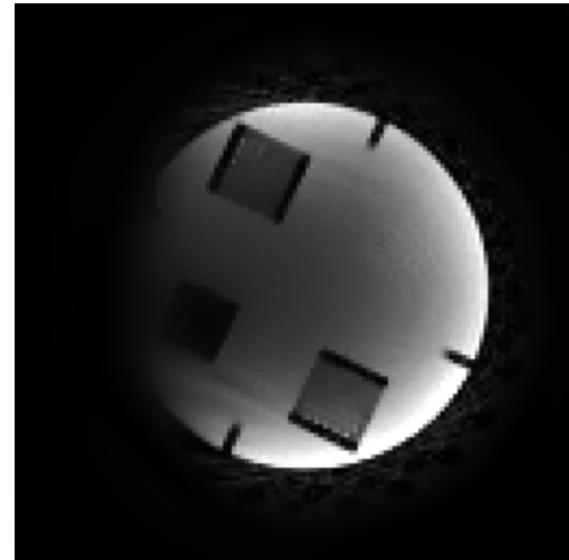


(b) IRGNTGV (detail)

# Radial sampling: phantom (25 proj)

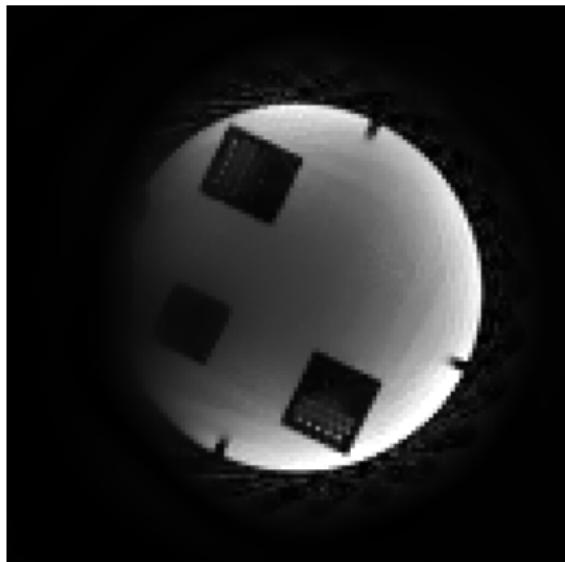


(a) IRGNTV

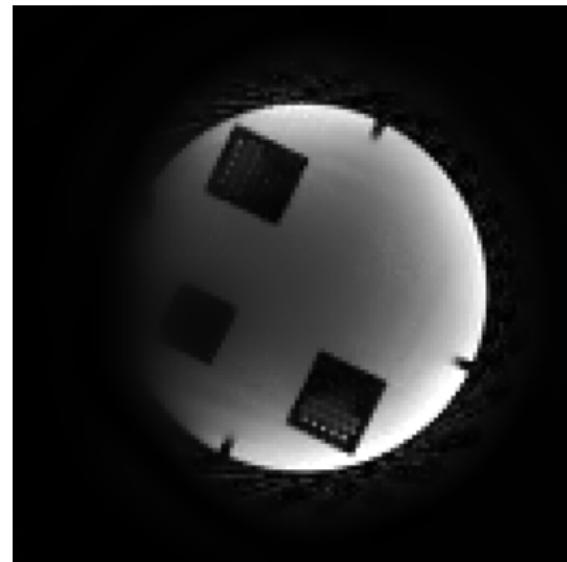


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

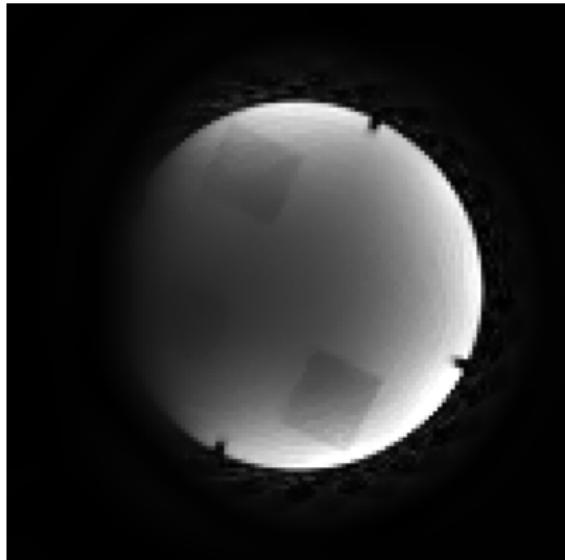


(a) IRGNTV

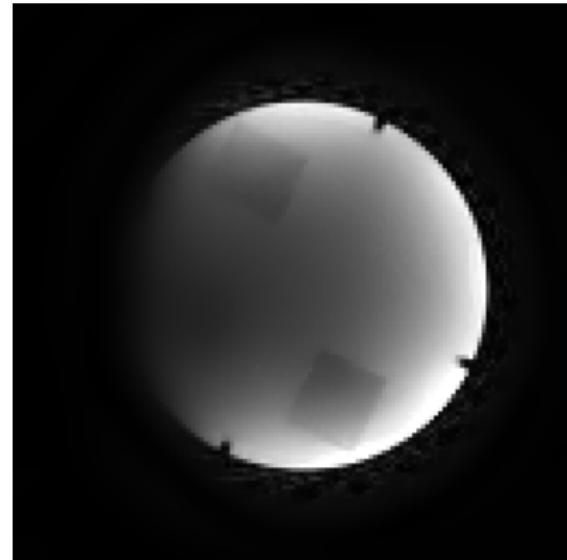


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

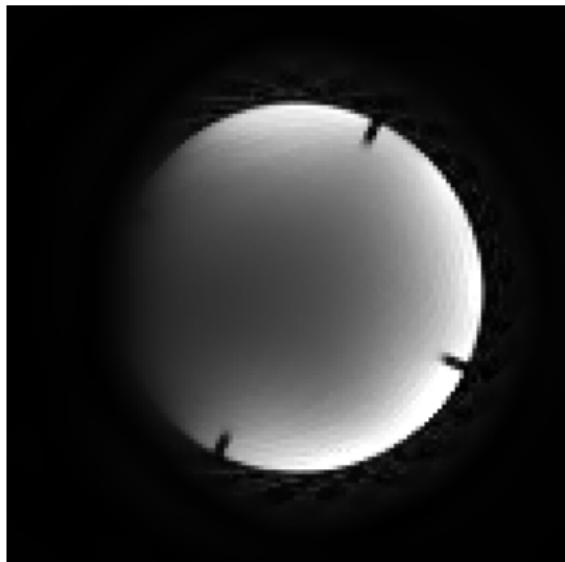


(a) IRGNTV

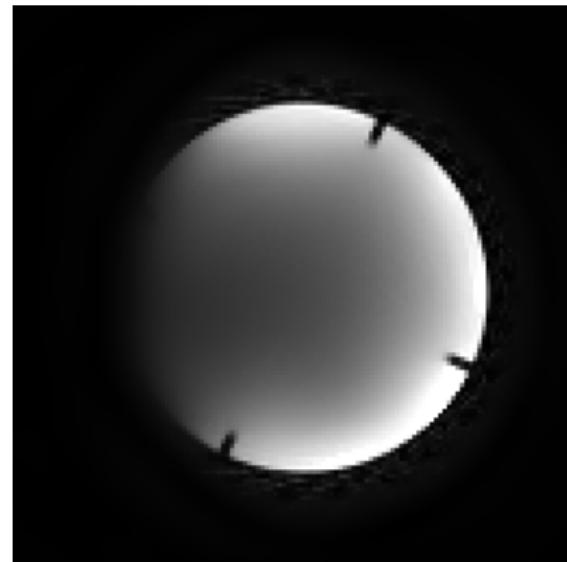


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

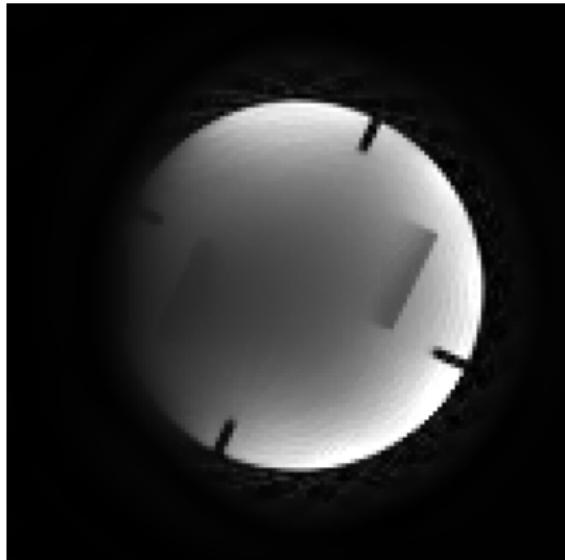


(a) IRGNTV

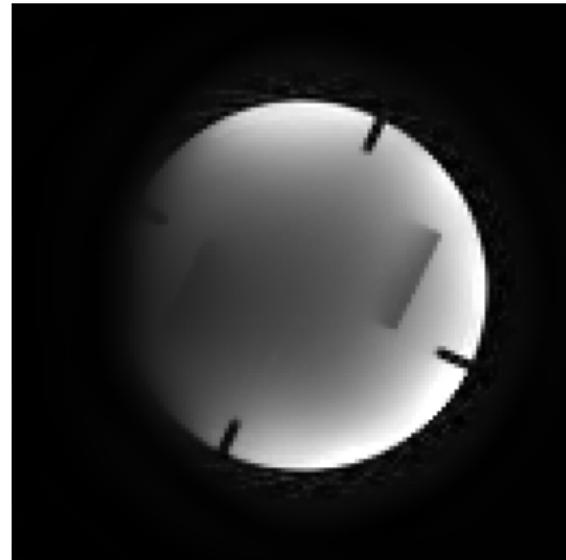


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

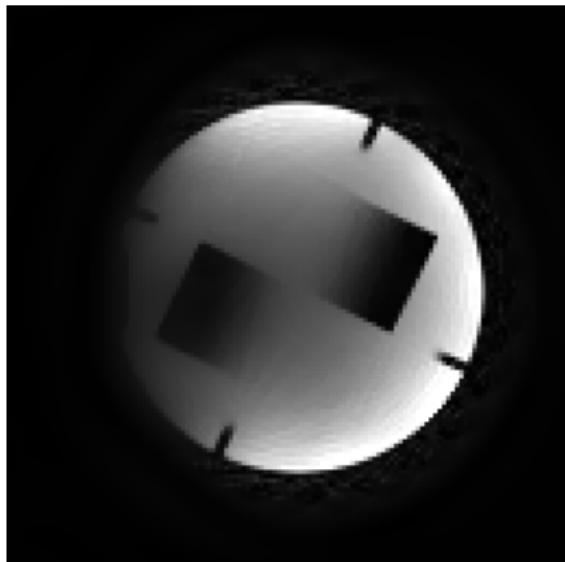


(a) IRGNTV



(b) IRGNTGV

# Radial sampling: phantom (25 proj)



(a) IRGNTV

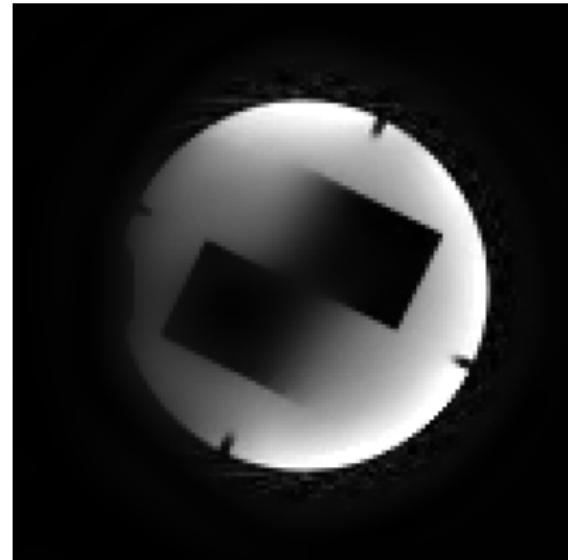


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

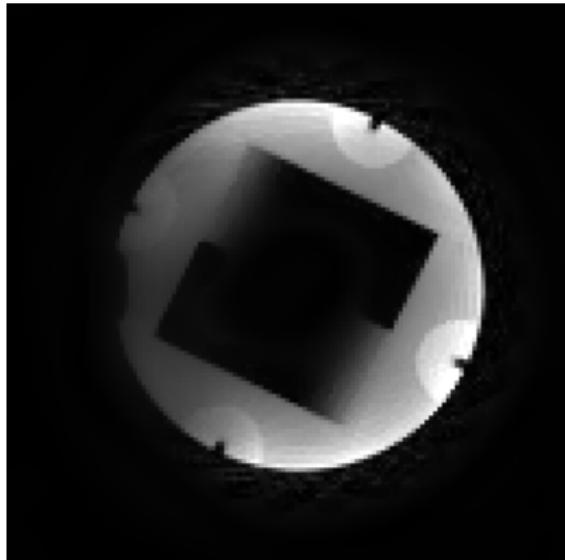


(a) IRGNTV

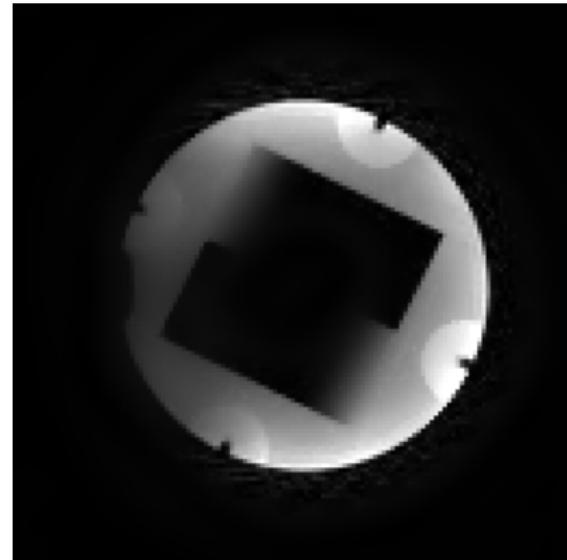


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

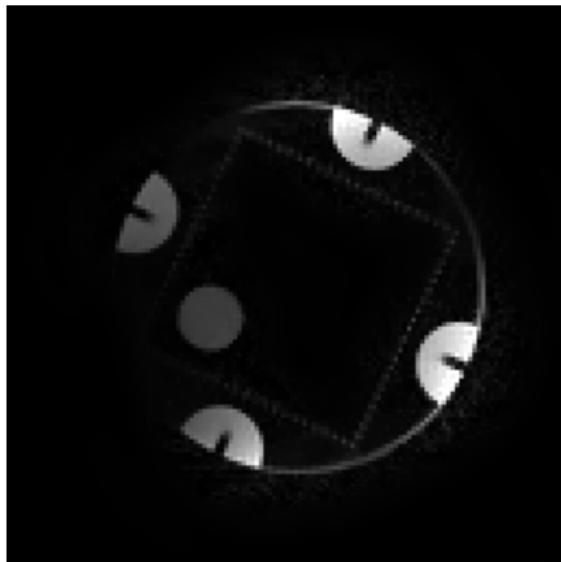


(a) IRGNTV

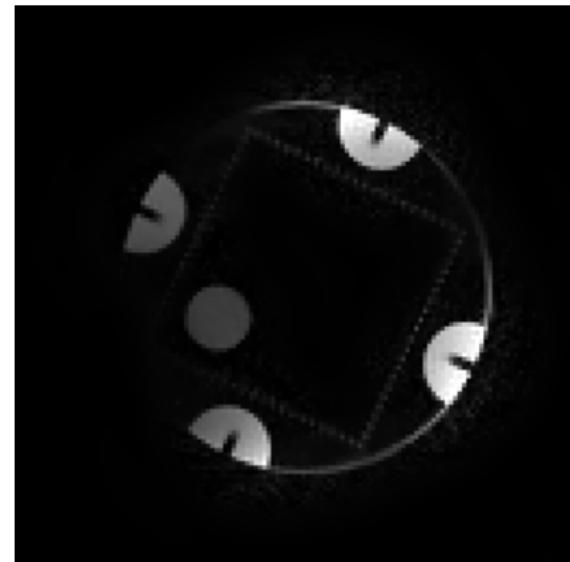


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

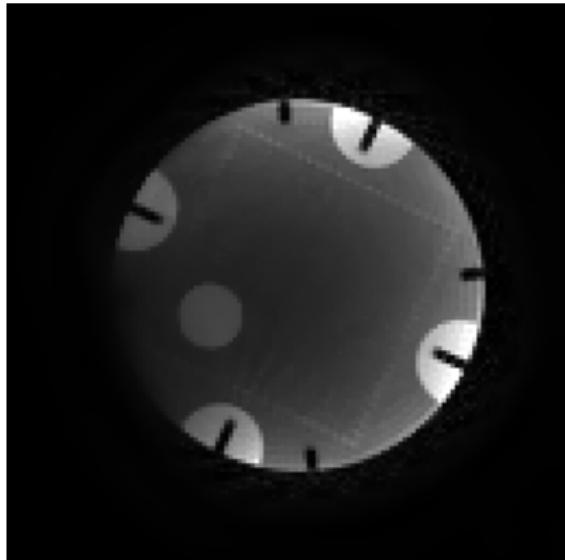


(a) IRGNTV

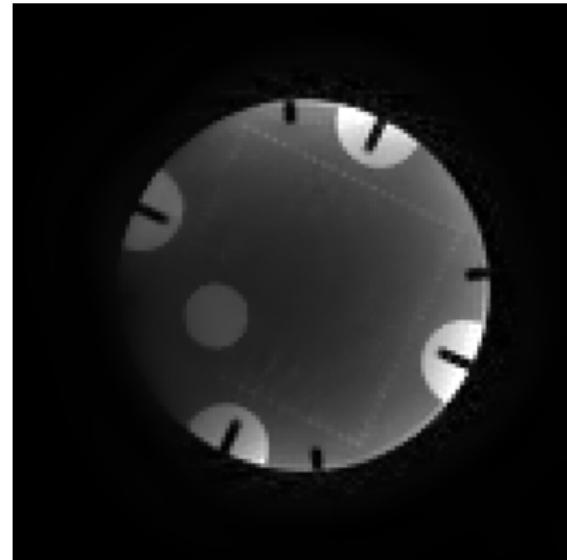


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

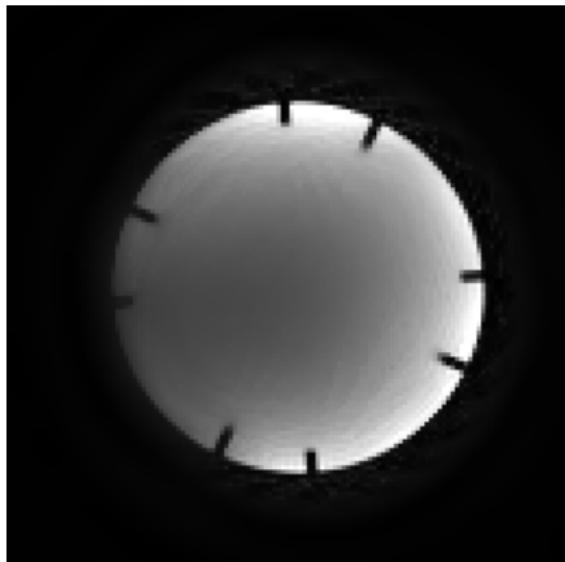


(a) IRGNTV

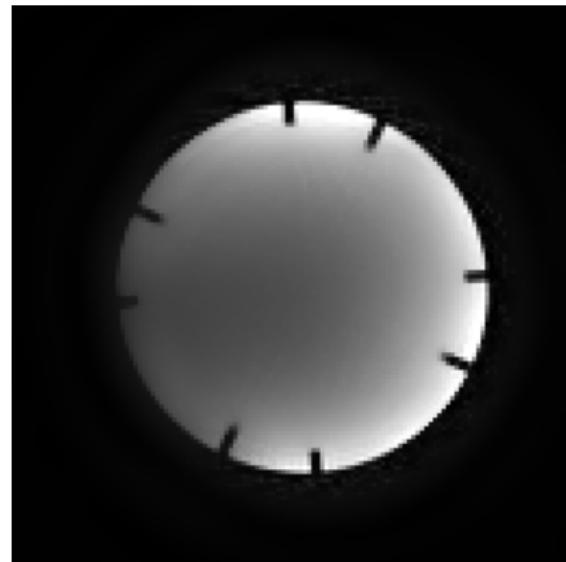


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

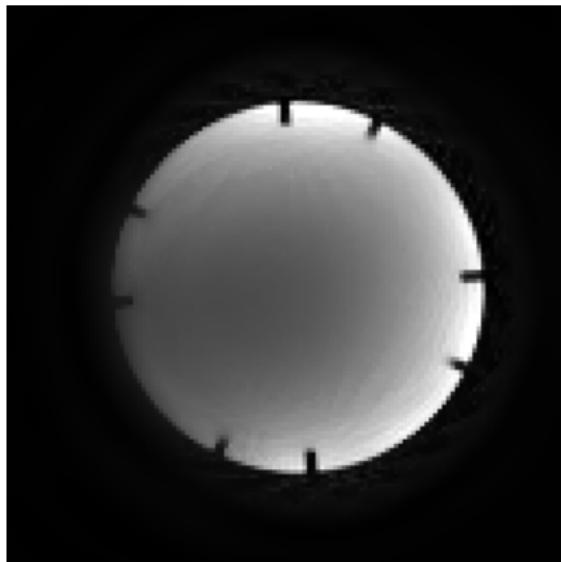


(a) IRGNTV

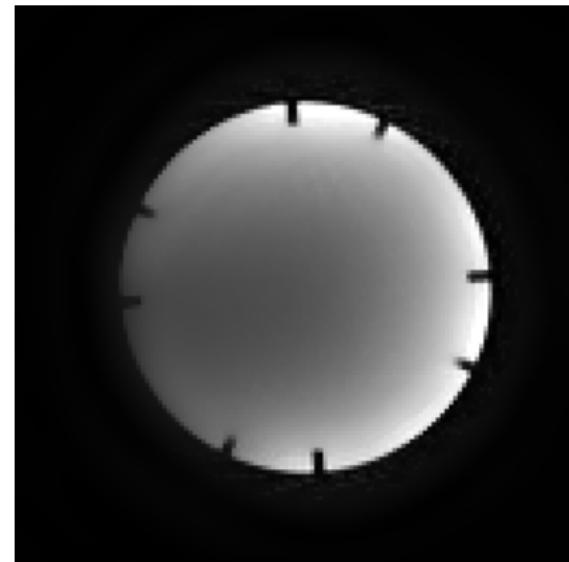


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

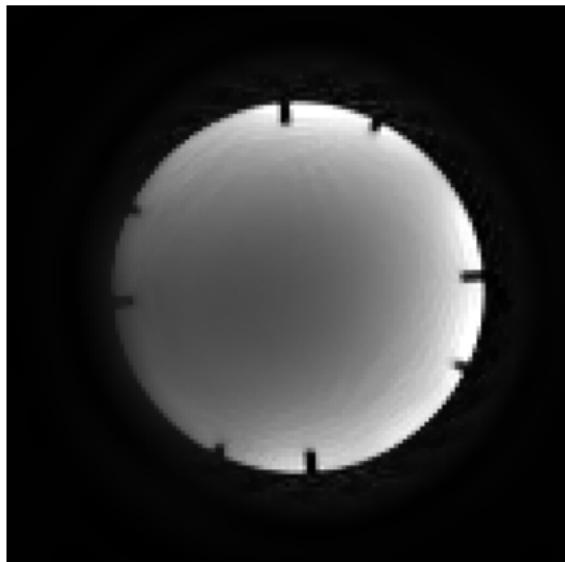


(a) IRGNTV

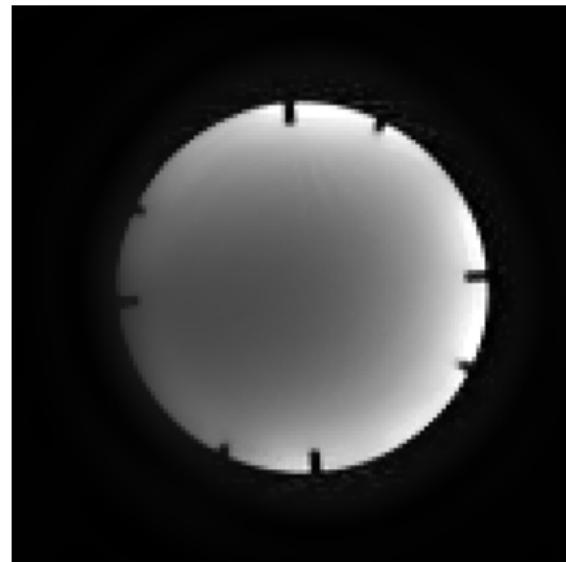


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

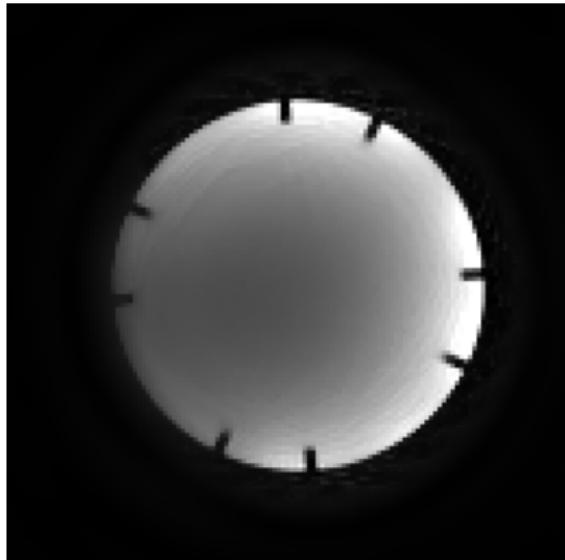


(a) IRGNTV

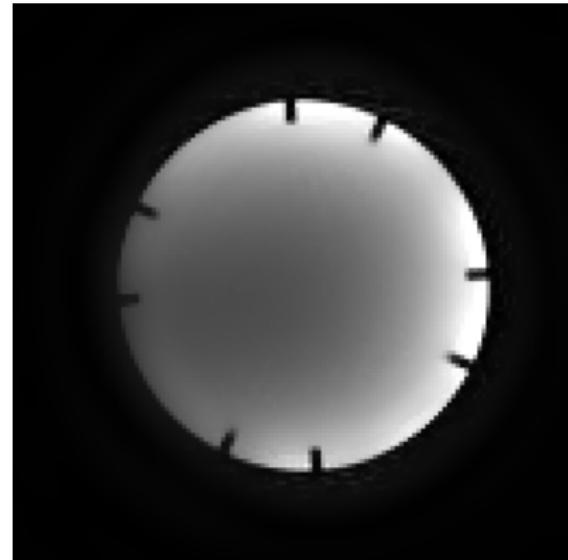


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

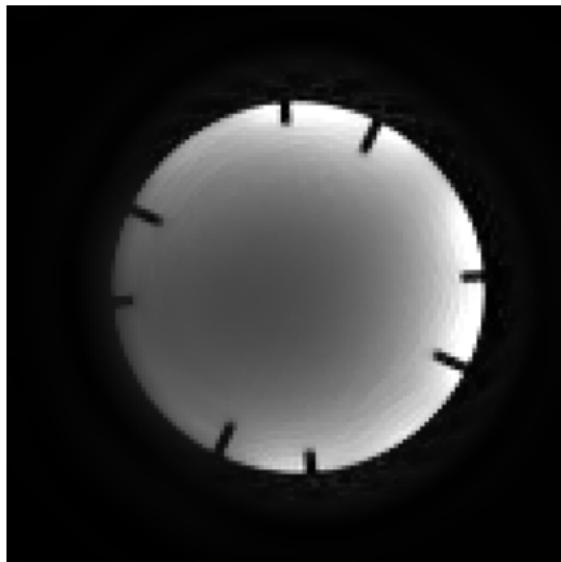


(a) IRGNTV

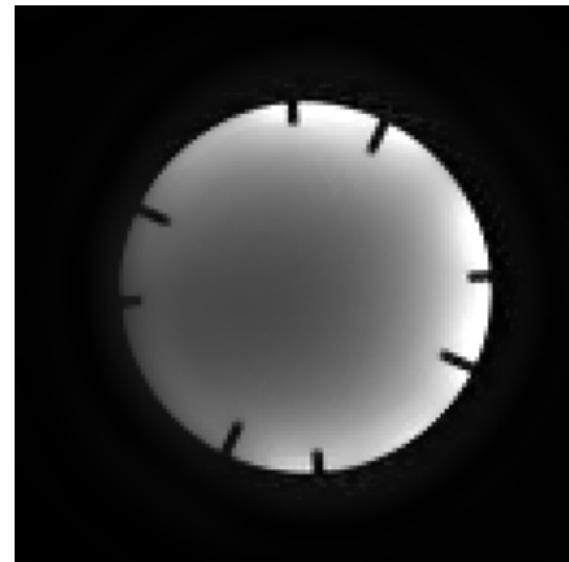


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

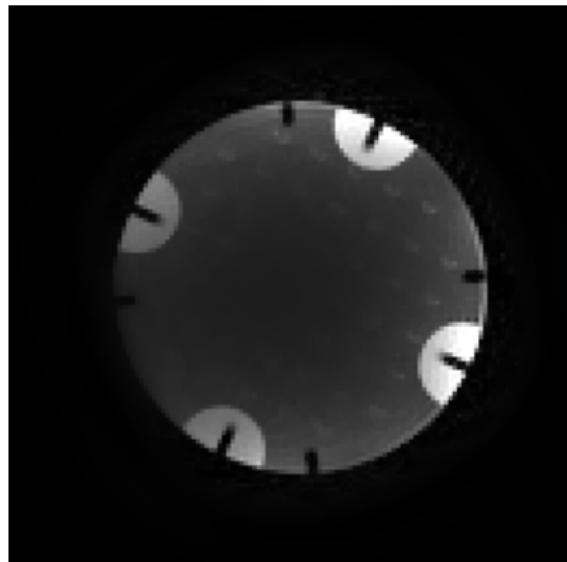


(a) IRGNTV

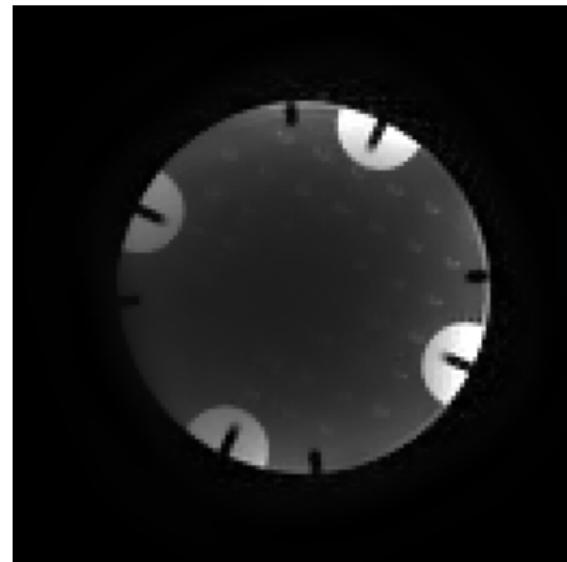


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

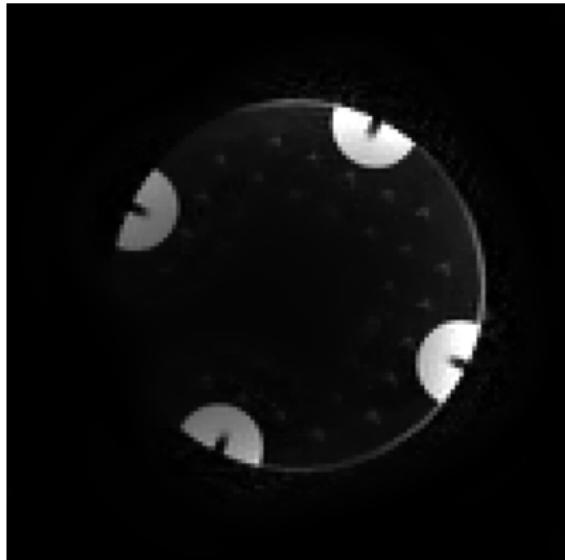


(a) IRGNTV

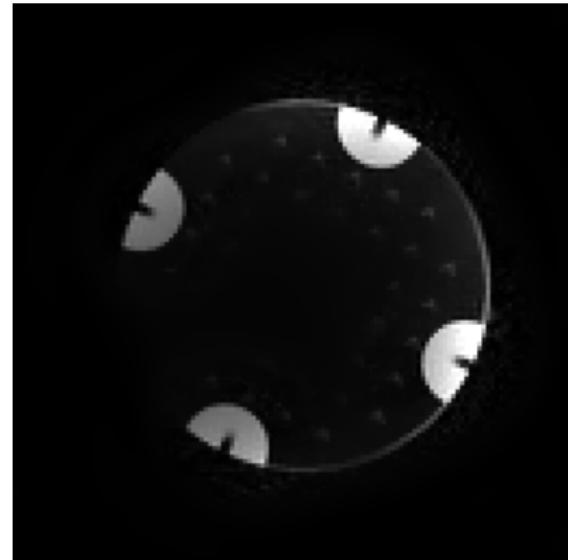


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

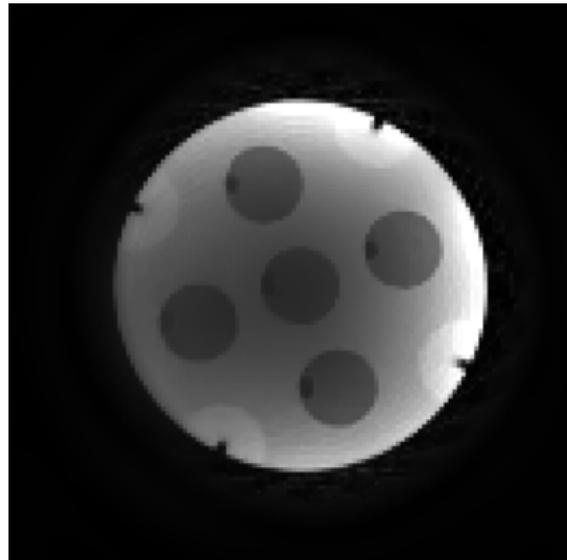


(a) IRGNTV

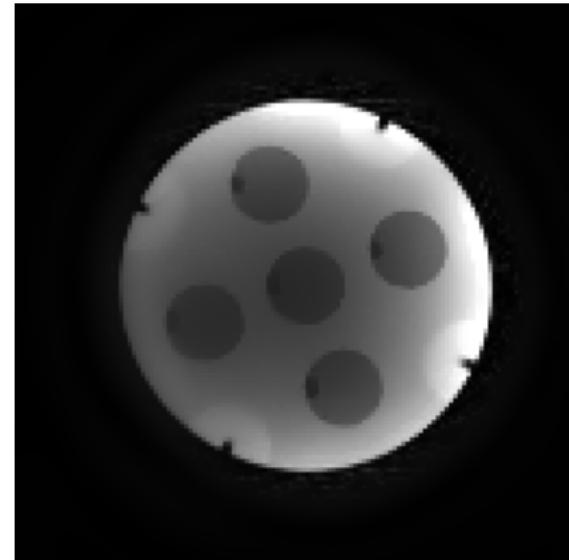


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

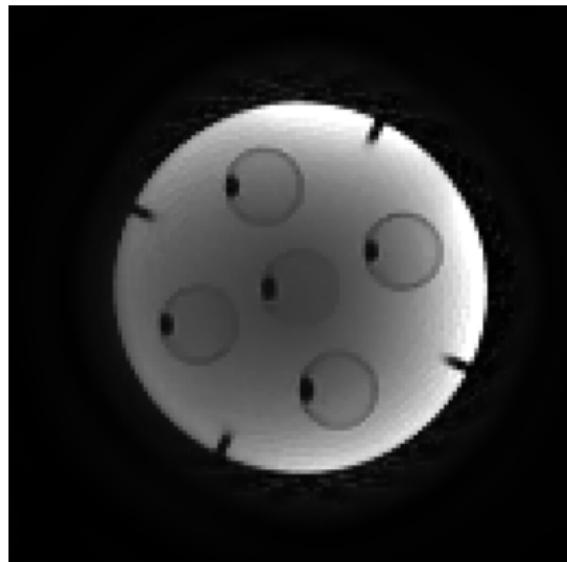


(a) IRGNTV

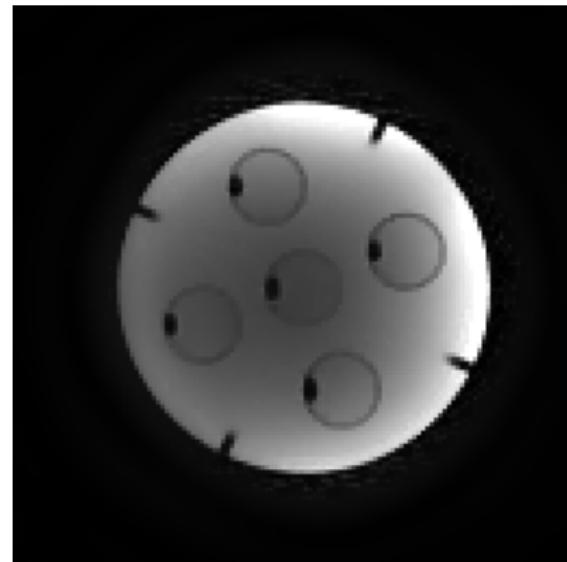


(b) IRGNTGV

# Radial sampling: phantom (25 proj)

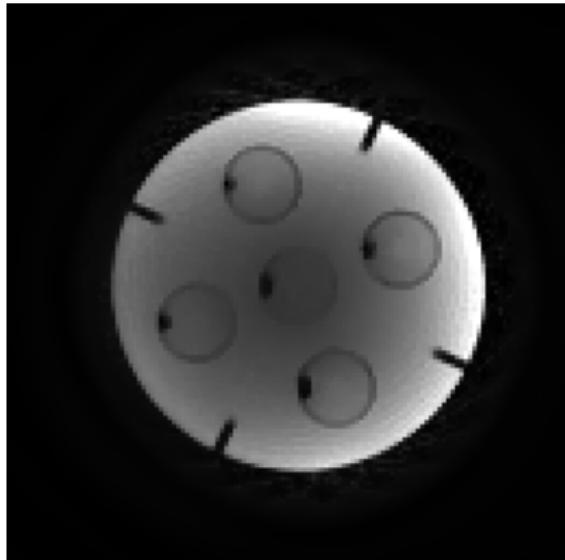


(a) IRGNTV

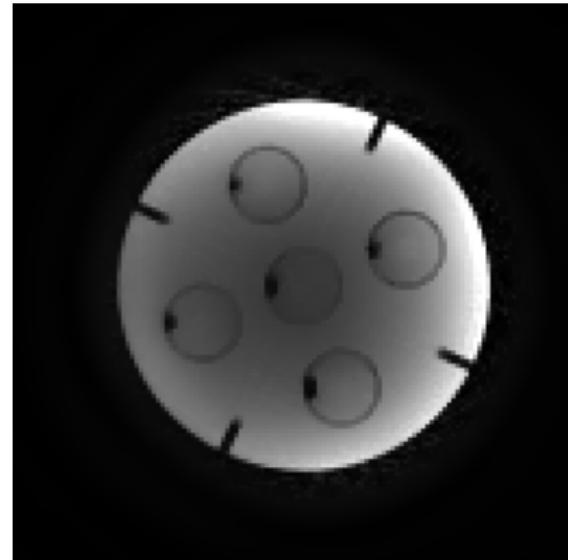


(b) IRGNTGV

# Radial sampling: phantom (25 proj)



(a) IRGNTV



(b) IRGNTGV

# Conclusion

## Summary:

- Nonlinear inverse approach gives flexibility
- IRGNTV more stable, same complexity as IRGN
- IRGNTGV better for modulated images

## Outlook:

- Add constraint on slice/frame differences; 3DT(G)V
- Include parameter identification in IRGN

Thanks to Martin Uecker (FLASH data), Kristian Bredies (TGV)

# Computation of gradients

$$J(\delta u, \delta c) = \frac{1}{2} \|F'(x)\delta x + F(x) - g\|^2 + \frac{\alpha}{2} \|W(c + \delta c)\|^2$$

$$\partial_u J(u, c)(\delta u, \delta c) = \sum_{i=1}^N c_i^* \cdot \mathcal{F}_s^*(\mathcal{F}_s(u \cdot \delta c_i + c_i \cdot \delta u) + F(u, c) - g)$$

$$(\partial_c J(u, c)(\delta u, \delta c))_i = u^* \cdot \mathcal{F}_s^*(\mathcal{F}_s(u \cdot \delta c_i + c_i \cdot \delta u) + F(u, c) - g) + \alpha W^* W(c_i + \delta c_i)$$

~~~ only (N)FFT, pointwise multiplication required

◀ back